

# Role of Imaging in Heart Failure Management

HKCC Core Cardiology Certificate Course Module 4

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# Imaging in Heart Failure

- Establish the diagnosis
- Assess etiology
- Determine prognosis
- Guide treatment

# Imaging in Heart Failure

- Structural abnormalities
- Function (systolic, diastolic, myocardial etc)
- Viability / ischaemia
- Scarring / fibrosis / infiltration

# Imaging in Heart Failure

- Echo
- Cardiac MRI
- Nuclear Imaging

# Echo

- “Ancient” technique
- Versatility
- Readily available
- Safe
- Lower cost
- But relatively high variability

## GUIDELINES AND STANDARDS

# Recommendations for Cardiac Chamber Quantification by Echocardiography in Adults: An Update from the American Society of Echocardiography and the European Association of Cardiovascular Imaging

Roberto M. Lang, MD, FASE, FESC, Luigi P. Badano, MD, PhD, FESC, Victor Mor-Avi, PhD, FASE, Jonathan Afilalo, MD, MSc, Anderson Armstrong, MD, MSc, Laura Ernande, MD, PhD, Frank A. Flachskampf, MD, FESC, Elyse Foster, MD, FASE, Steven A. Goldstein, MD, Tatiana Kuznetsova, MD, PhD, Patrizio Lancellotti, MD, PhD, FESC, Denisa Muraru, MD, PhD, Michael H. Picard, MD, FASE, Ernst R. Rietzschel, MD, PhD, Lawrence Rudski, MD, FASE, Kirk T. Spencer, MD, FASE, Wendy Tsang, MD, and Jens-Uwe Voigt, MD, PhD, FESC, *Chicago, Illinois; Padua, Italy; Montreal, Quebec and Toronto, Ontario, Canada; Baltimore, Maryland; Créteil, France; Uppsala, Sweden; San Francisco, California; Washington, District of Columbia; Leuven, Liège, and Ghent, Belgium; Boston, Massachusetts*

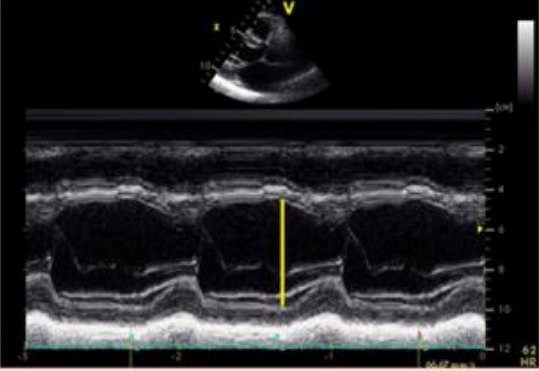

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The rapid technological developments of the past decade and the changes in echocardiographic practice brought about by these developments have resulted in the need for updated recommendations to the previously published guidelines for cardiac chamber quantification, which was the goal of the joint writing group assembled by the American Society of Echocardiography and the European Association of Cardiovascular Imaging. This document provides updated normal values for all four cardiac chambers, including three-dimensional echocardiography and myocardial deformation, when possible, on the basis of considerably larger numbers of normal subjects, compiled from multiple databases. In addition, this document attempts to eliminate several minor discrepancies that existed between previously published guidelines. (J Am Soc Echocardiogr 2015;28:1-39.)

**Keywords:** Adult echocardiography, Transthoracic echocardiography, Ventricular function, Normal values

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# M-mode vs 2D

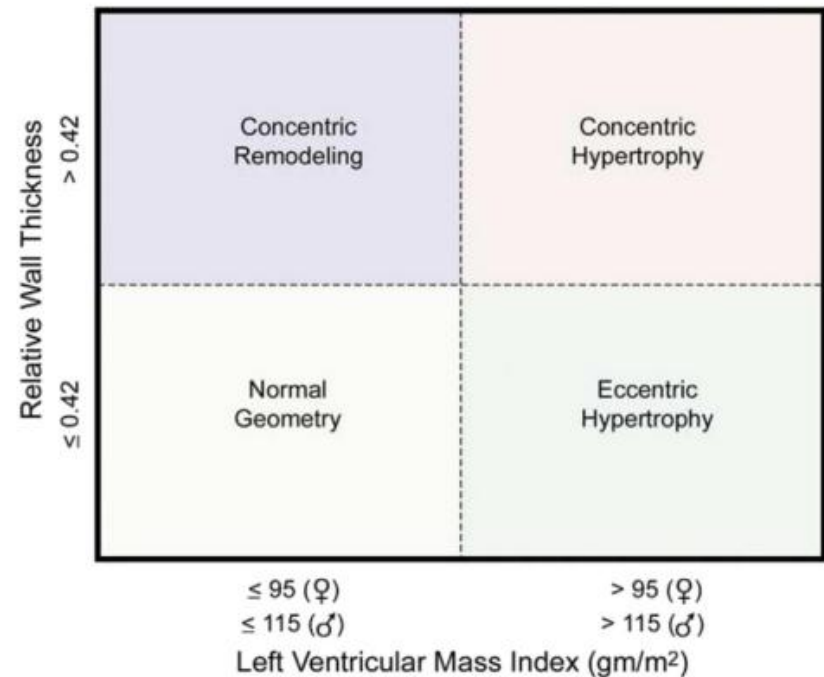
Parameter and method	Technique	Advantages	Limitations
<p><b>Internal linear dimensions.</b></p> <p>Linear internal measurements of the LV should be acquired in the parasternal long-axis view carefully obtained perpendicular to the LV long axis, and measured at the level of the mitral valve leaflet tips. Electronic calipers should be positioned on the interface between myocardial wall and cavity and the interface between wall and pericardium (<i>orange arrows</i>).</p>	<p>M-mode tracing</p>  <p>2D-guided linear measurements</p> 	<ul style="list-style-type: none"> <li>• Reproducible</li> <li>• High temporal resolution</li> <li>• Wealth of published data</li> </ul> <ul style="list-style-type: none"> <li>• Facilitates orientation perpendicular to the ventricular long axis</li> </ul>	<ul style="list-style-type: none"> <li>• Beam orientation frequently off axis</li> <li>• Single dimension, i.e., representative only in normally shaped ventricles</li> </ul> <ul style="list-style-type: none"> <li>• Lower frame rates than M-mode</li> <li>• Single dimension, i.e., representative only in normally shaped ventricles</li> </ul>

# LV wall thickness and geometry

**Table 6** Normal ranges for LV mass indices

	Women	Men
Linear method		
LV mass (g)	67–162	88–224
<b><i>LV mass/BSA (<math>g/m^2</math>)</i></b>	<b><i>43–95</i></b>	<b><i>49–115</i></b>
Relative wall thickness (cm)	0.22–0.42	0.24–0.42
<b><i>Septal thickness (cm)</i></b>	<b><i>0.6–0.9</i></b>	<b><i>0.6–1.0</i></b>
<b><i>Posterior wall thickness (cm)</i></b>	<b><i>0.6–0.9</i></b>	<b><i>0.6–1.0</i></b>
2D method		
LV mass (g)	66–150	96–200
<b><i>LV mass/BSA (<math>g/m^2</math>)</i></b>	<b><i>44–88</i></b>	<b><i>50–102</i></b>

Bold italic values: recommended and best validated.



**Figure 6** Comparison of RWT. Patients with normal LV mass can have either concentric remodeling (normal LV mass with increased RWT  $\geq 0.42$ ) or normal geometry (RWT  $\leq 0.42$ ) and normal LV mass. Patients with increased LV mass can have either concentric (RWT  $\geq 0.42$ ) or eccentric (RWT  $\leq 0.42$ ) hypertrophy. These LV mass measurements are based on linear measurements.



# LV EF (ejection fraction)

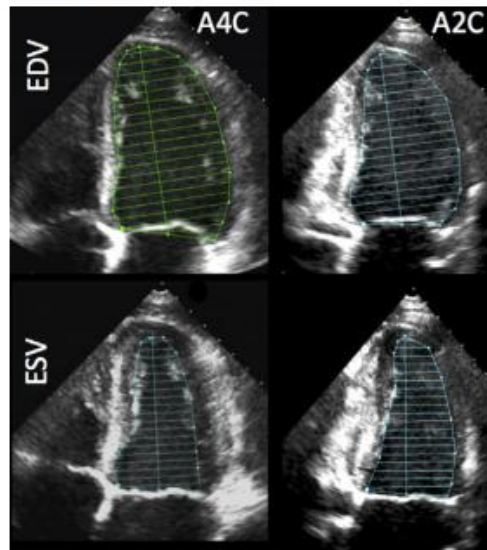
- Most commonly (and firstly) asked question by both physicians and patients
- A “number” that provides a general impression how “good” or “bad” one’s heart is – “easy to understand”
- Important for cardiologists to determine timing of intervention (e.g. CRT-P/D, valvular surgery in severe lesions)

# Volume and EF assessment

## Volumes.

Volume measurements are usually based on tracings of the blood-tissue interface in the apical four- and two-chamber views. At the mitral valve level, the contour is closed by connecting the two opposite sections of the mitral ring with a straight line. LV length is defined as the distance between the middle of this line and the most distant point of the LV contour.

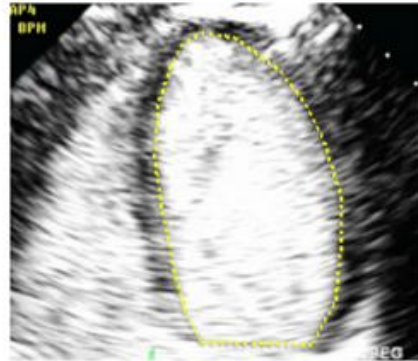
## Biplane disk summation



- Corrects for shape distortions
- Less geometrical assumptions compared with linear dimensions
- Apex frequently foreshortened
- Endocardial dropout
- Blind to shape distortions not visualized in the apical two- and four-chamber planes

# Volume and EF assessment

Endocardial border enhancement



- Helpful in patients with suboptimal acoustic window
- Provides volumes that are closer to those measured with cardiac magnetic resonance
- Same limitations as the above non-contrast 2D techniques
- Acoustic shadowing in LV basal segments with excess contrast

3D data sets



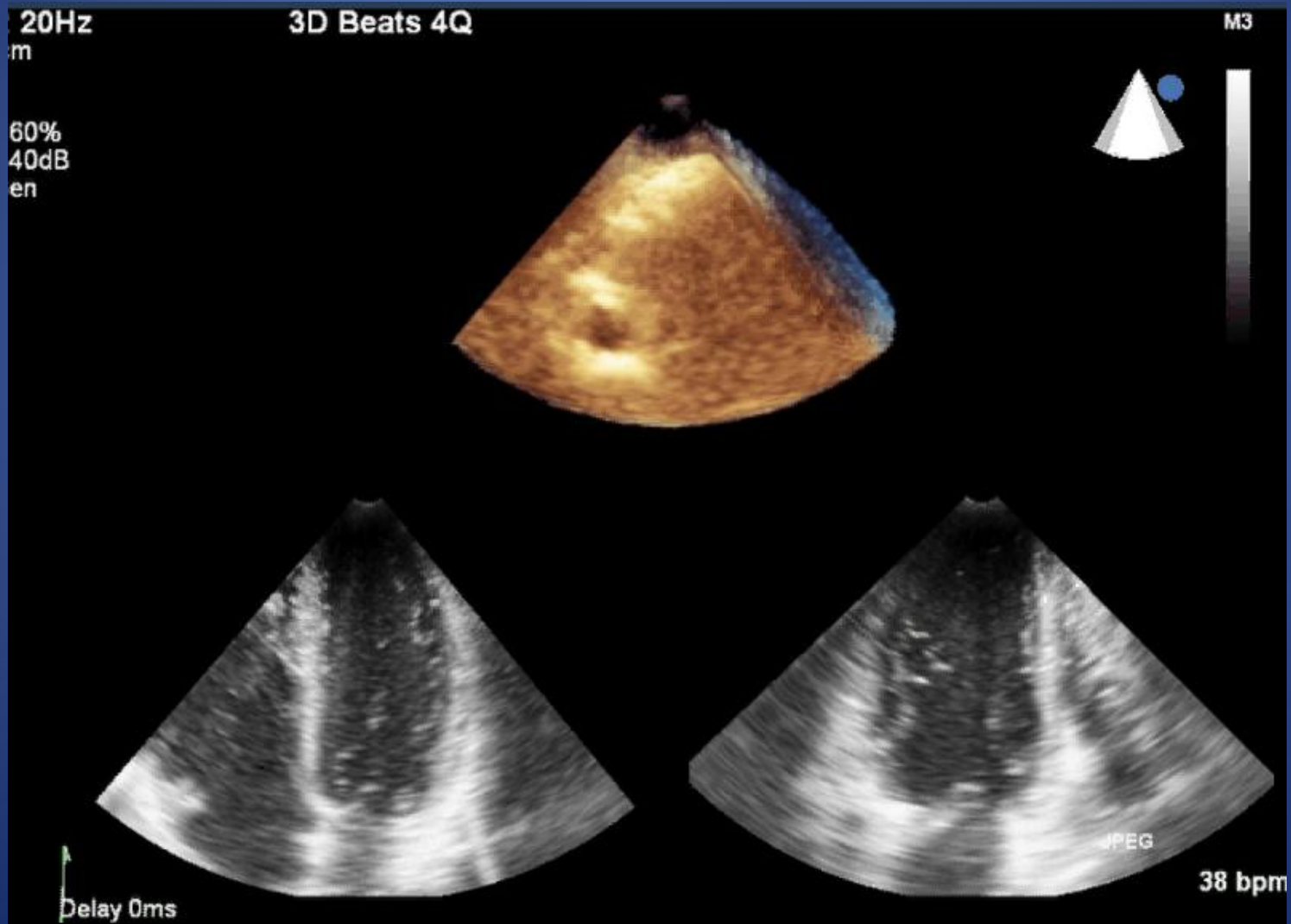
- No geometrical assumption
- Unaffected by foreshortening
- More accurate and reproducible compared to other imaging modalities
- Lower temporal resolution
- Less published data on normal values
- Image quality dependent

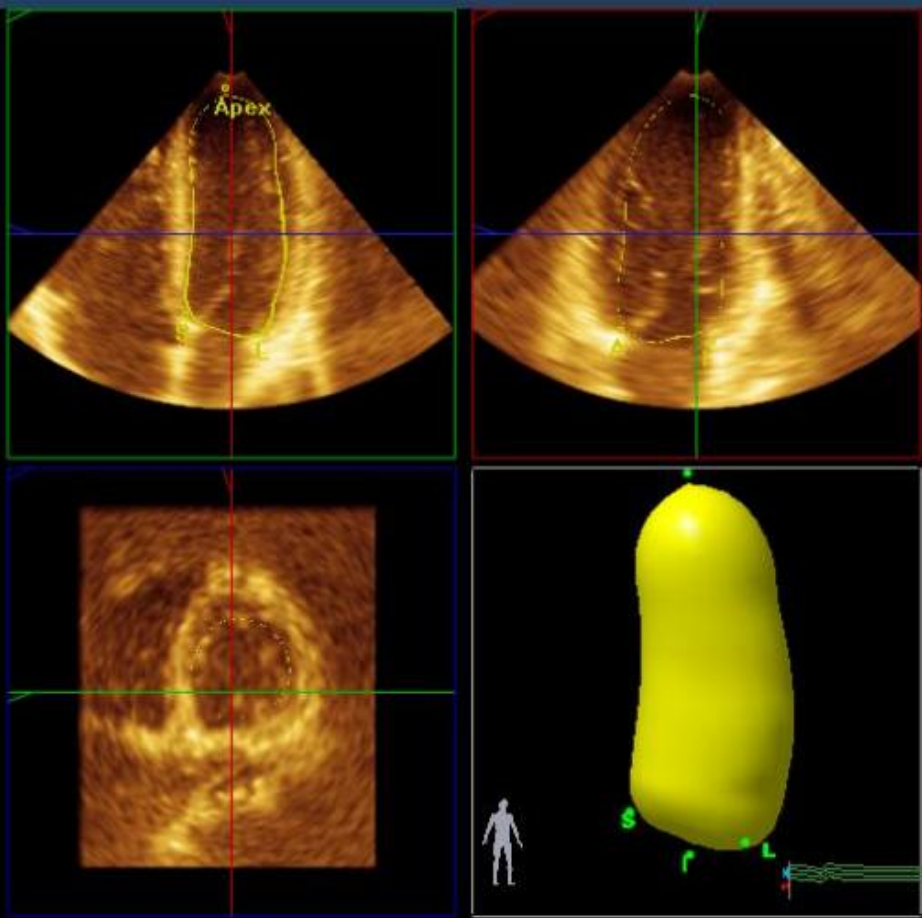
# LVEF vs Cardiac Output

- $CO = HR \times SV$
- $EF (\%) = SV / LV \text{ end diastolic volume}$
- **Assuming that no significant mitral regurgitation**
- **$CO = HR \times (EF (\%) \times LV \text{ end diastolic volume})$**



# 3D full volume acquisition





Volume(s)

EDV = 84.7 ml

ESV = 27.4 ml

Calculation(s)

EF = 67.6 %

SV = 57.3 ml

Regional

Tmsv Sel-SD = ~~####~~

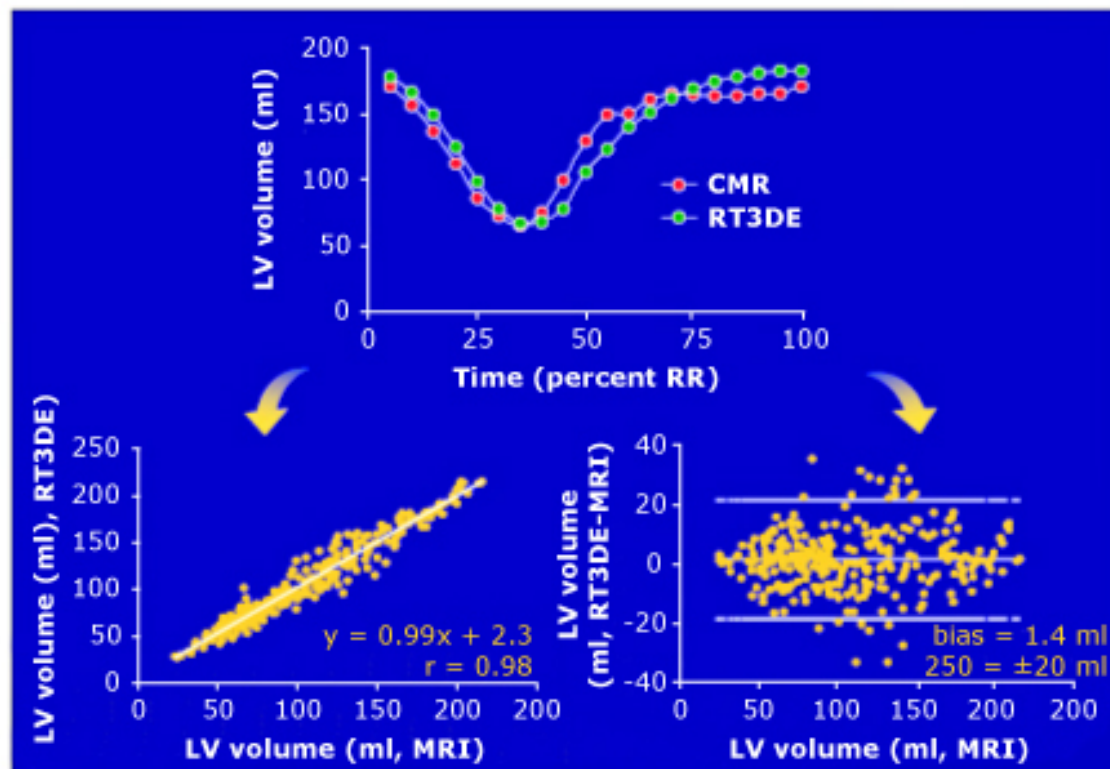
Tmsv Sel-Dif = ~~####~~

Tmsv Sel-SD = ~~####~~



Global Regional Normalized

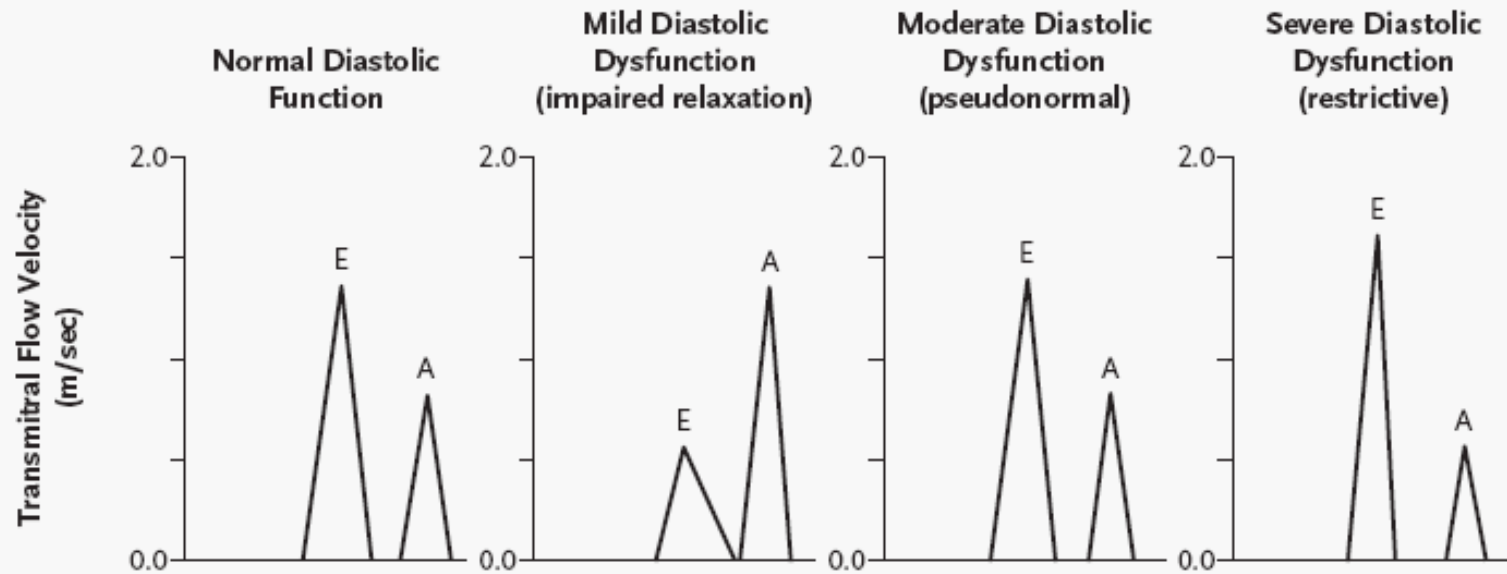
## Accuracy of real time three-dimensional echocardiography (RT3DE) measurements of left ventricular (LV) volume



Example of LV volume time curves obtained in one patient from RT3DE and MR images. Results of linear regression (bottom, left) and Bland-Altman (bottom, right) analyses of the point-by-point measurements of LV volume obtained in 16 patients.

*Corsi C, Lang RM, Veronesi F, et al. Volumetric quantification of global and regional left ventricular function from real-time three-dimensional echocardiographic images. Circulation 2005; 112:1161.*

# Diastolic function: Mitral inflow pattern



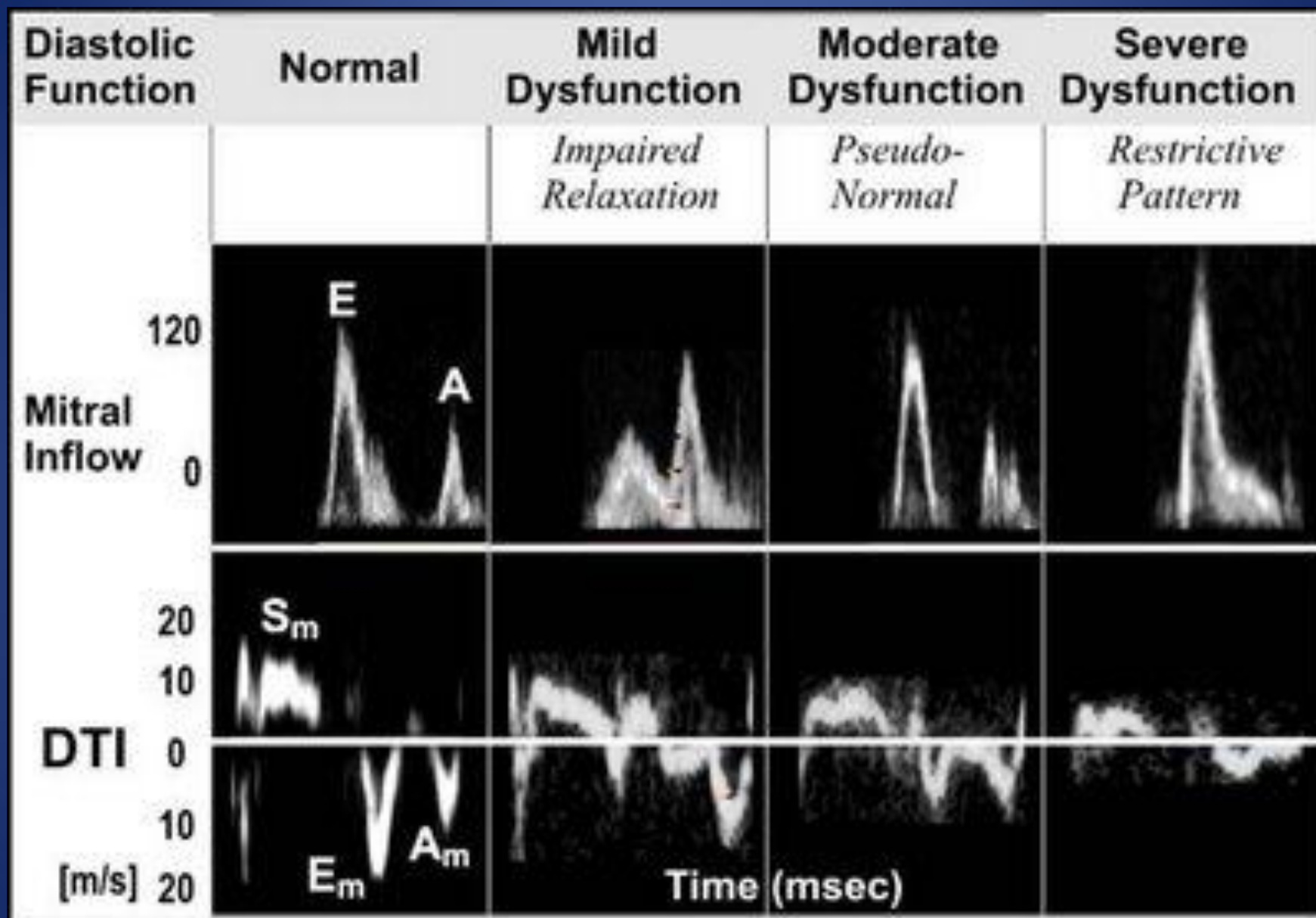
Left Ventricular Relaxation	Normal	Impaired	Impaired	Impaired
Left Ventricular Compliance	Normal	Normal to ↓	↓↓	↓↓↓
Atrial Pressure	Normal	Normal to ↑	↑↑	↑↑↑

E = early filling

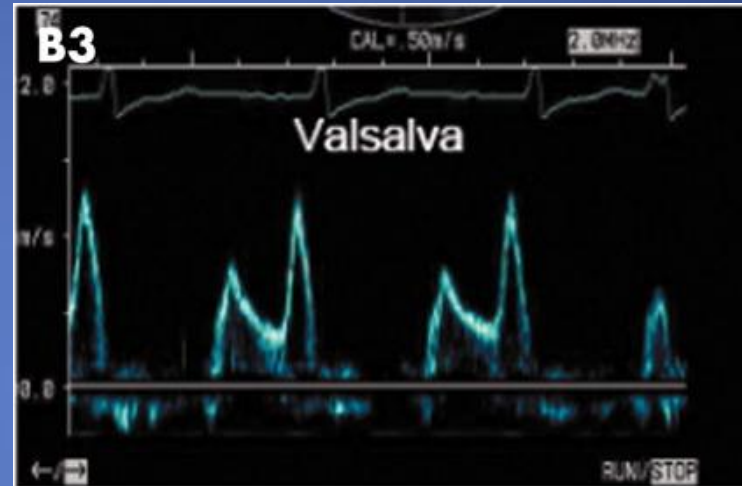
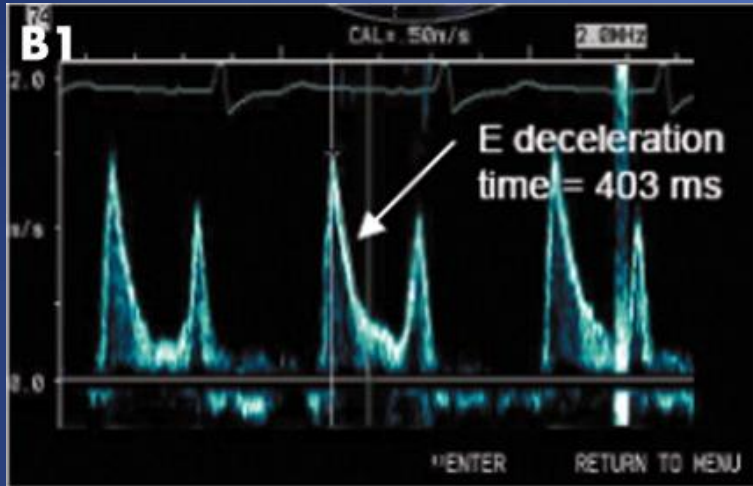
A = atrial contraction

Aurigemma GP. NEJM. 2004;351:1097-105.



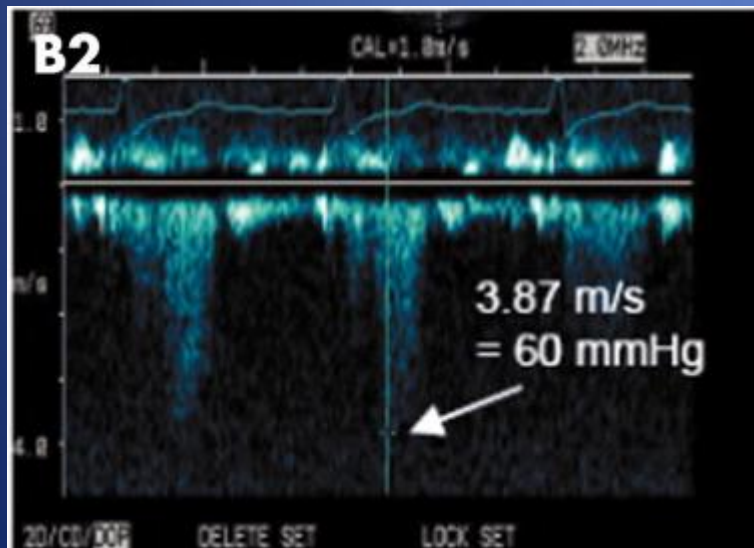


# Pseudonormal (grade 2) vs Normal

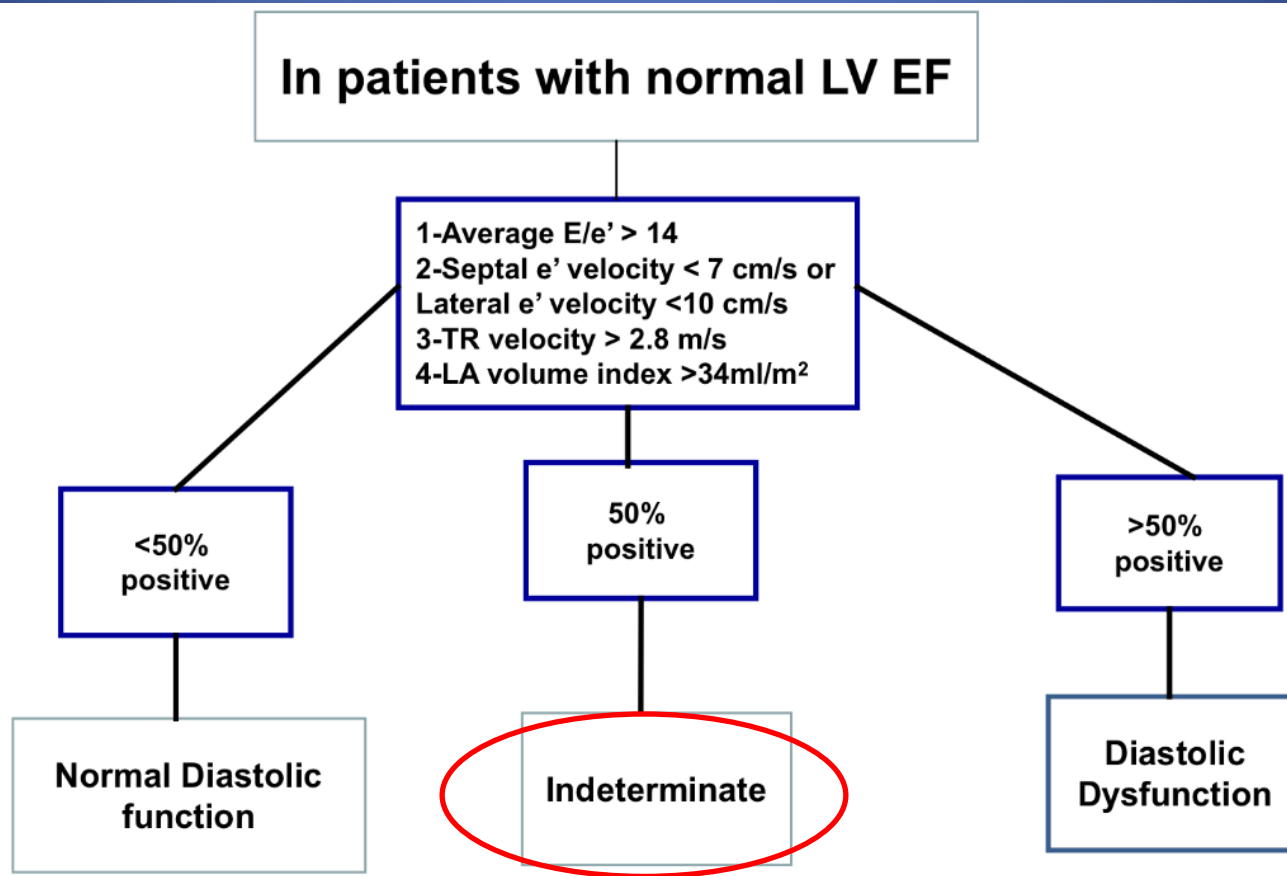


Valsalva – decrease preload and convert the mitral inflow into “abnormal relaxation pattern”

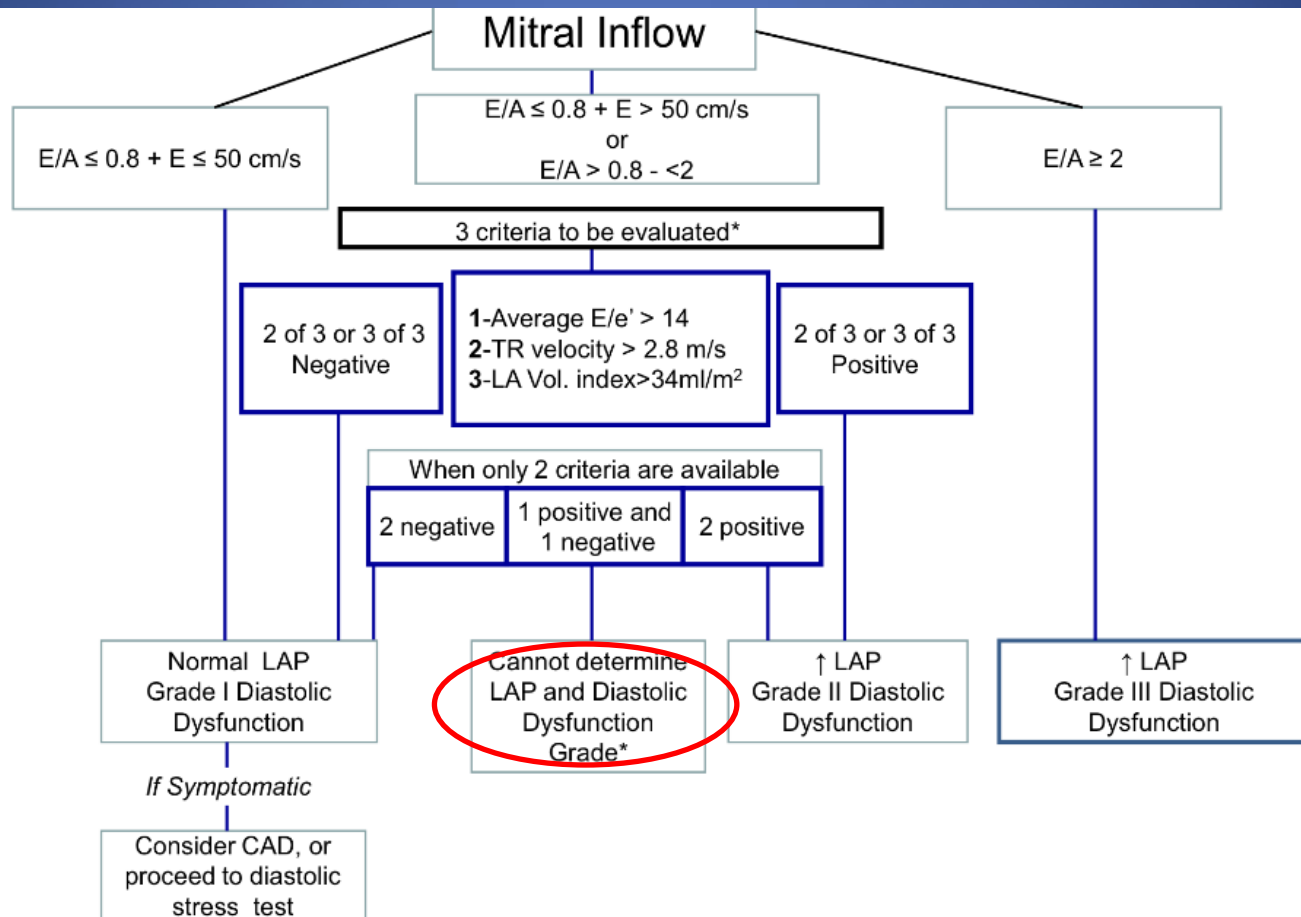
Pulmonary hypertension usually present



# Diagnosis of LV diastolic dysfunction in patients with normal LV EF



# Estimation of LV filling pressure/diastolic function grading in patient with depressed LVEF or myocardial disease

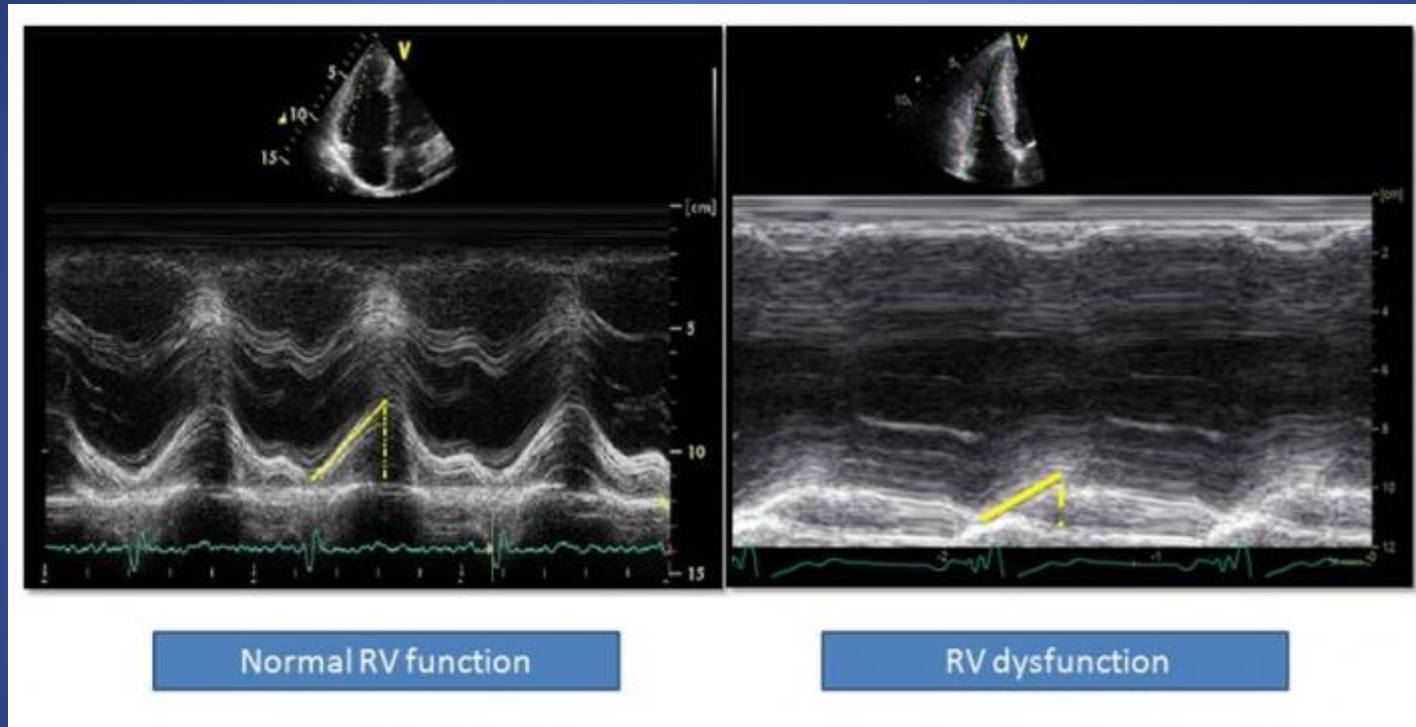


(\* : LAP indeterminate if only 1 of 3 parameters available. Pulmonary vein S/D ratio <1 applicable to conclude elevated LAP in patients with depressed LV EF)

# RV Geometry

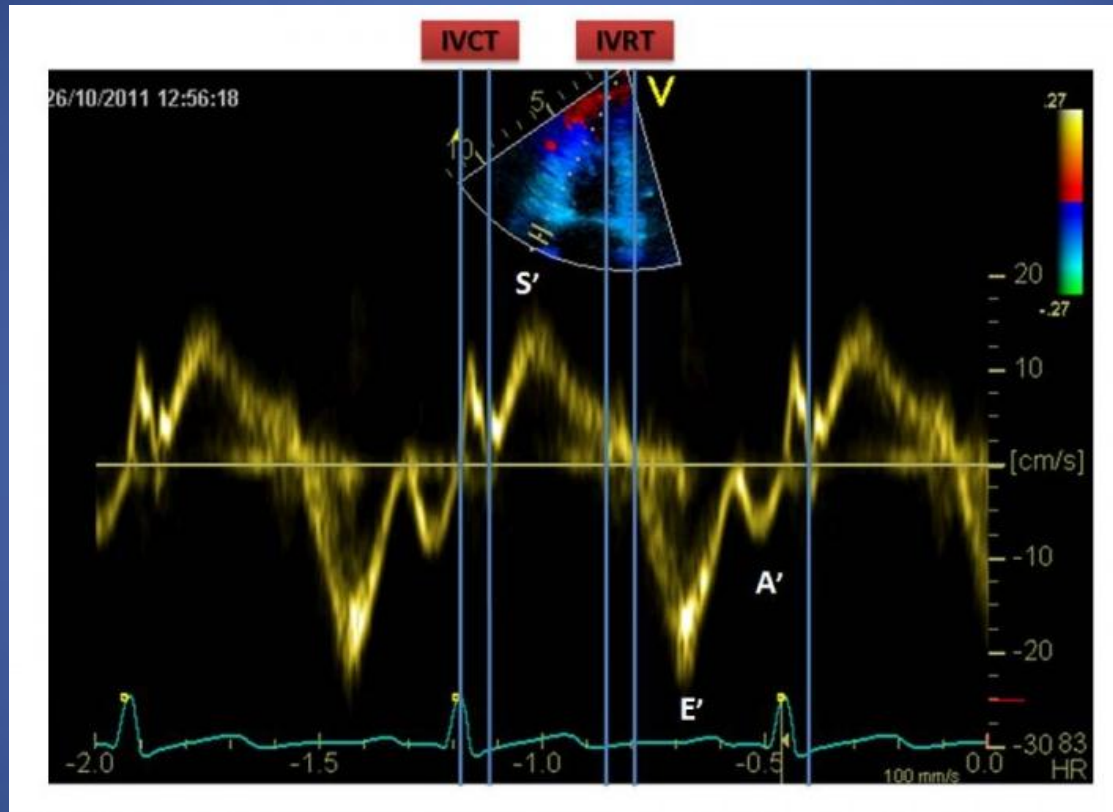
- The shape of the right ventricle is complex
- In contrast to the ellipsoidal shape of the left ventricle, the right ventricle is triangular when viewed longitudinally and is crescent shaped when viewed transversally.
- Its complex shape is difficult to model geometrically as opposed to the left ventricle, which explains the difficulty to assess right ventricular volumes and function by echocardiography

# Tricuspid Annular Plane Systolic Excursion (TAPSE)



- M-mode cursor passed through the tricuspid lateral annulus in a four-chamber view and measuring the amount of longitudinal displacement of the annulus at peak-systole
- Abnormal  $< 16$  mm

# Systolic Excursion velocity (S')



- Utilize Tissue Doppler Imaging of tricuspid annulus movement during systole
- Abnormal  $< 10$  cm/sec

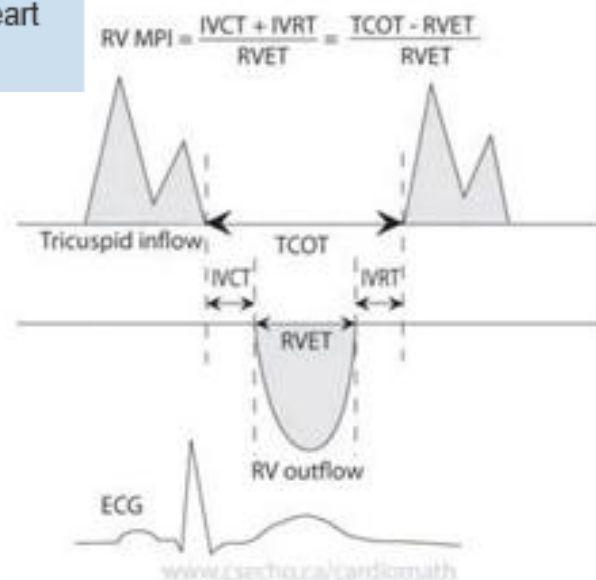
# RV Myocardial Performance Index

## RV MPI Abnormal Values

	Abnormal
Pulsed Doppler RV MPI	>0.40
Tissue Doppler RV MPI	>0.55

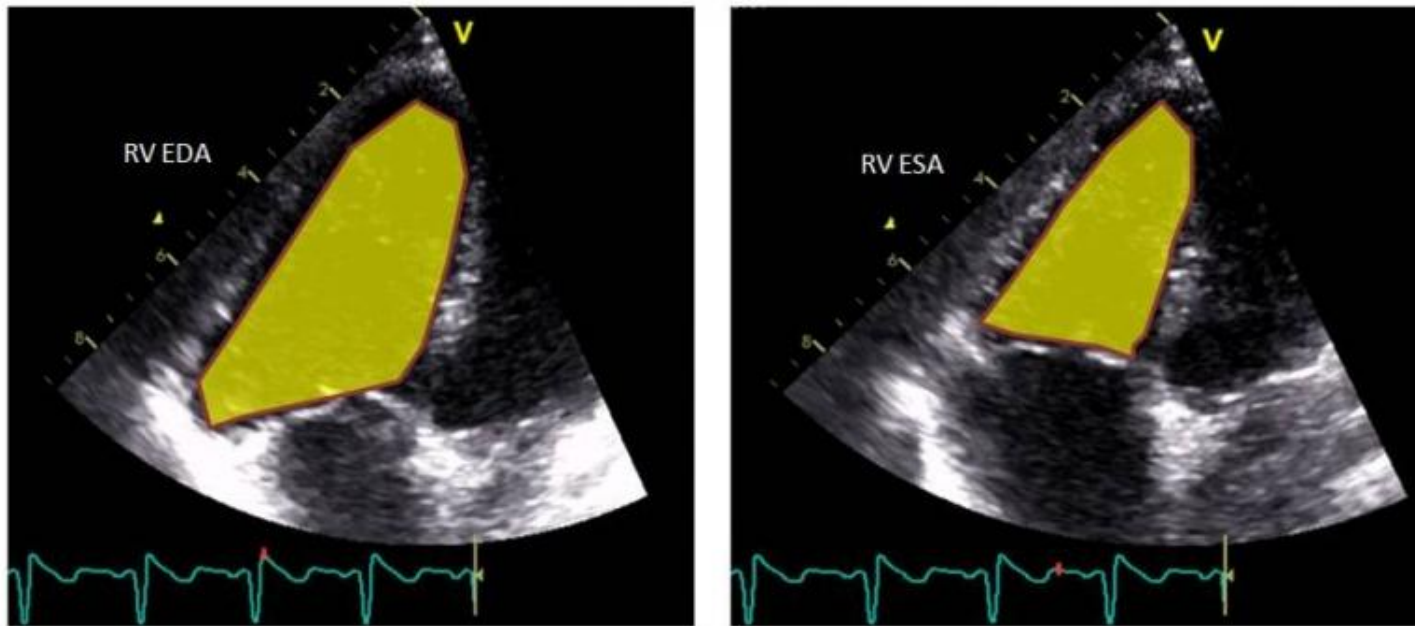
## RV MPI

Also known as RIMP or Tei index. It is an index that incorporates both systolic and diastolic time intervals in expressing global systolic and diastolic ventricular function. The RV MPI has prognostic value among pulmonary hypertension patients at a single point in time and changes in this index correlate with change in clinical status. It also been used in studying patients with RV infarction, hypertrophic cardiomyopathy, and congenital heart disease, etc.





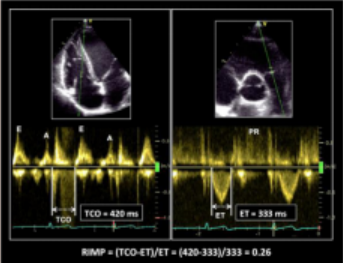
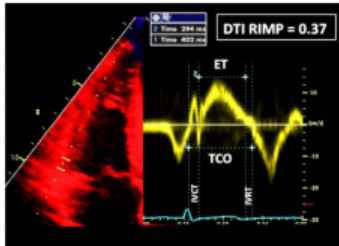
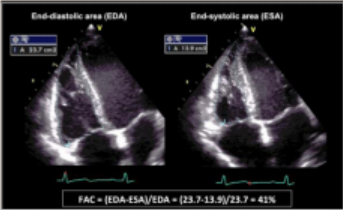
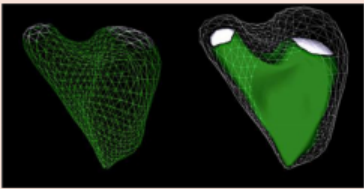
# Fractional Area Change



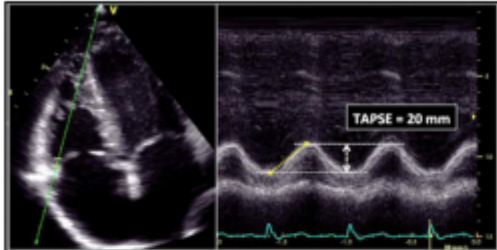
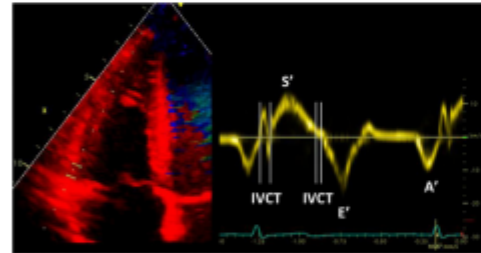
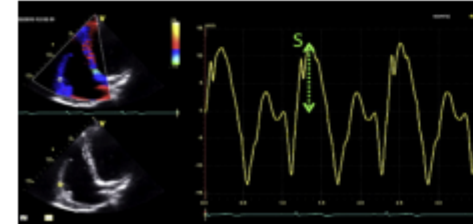
$$\text{RV FAC \%} = (\text{RV EDA} - \text{RV ESA}) / \text{RV EDA} \times 100$$

- Resemble “Simpons method” for LVEF
- Abnormal: < 35% change in area

**Table 9** Recommendations for the echocardiographic assessment of RV function

Echocardiographic imaging	Recommended methods	Advantages	Limitations
<p><b>RV global function</b> Pulsed Doppler RIMP</p> 	<p>RIMP (Tei index) by pulsed Doppler:  <math>RIMP = (TCO - ET)/ET</math></p>	<ul style="list-style-type: none"> <li>• Prognostic value</li> <li>• Less affected by heart rate</li> </ul>	<ul style="list-style-type: none"> <li>• Requires matching for R-R intervals when measurements are performed on separate recordings</li> <li>• Unreliable when RA pressure is elevated</li> </ul>
<p>Tissue Doppler RIMP</p> 	<p>RIMP by tissue Doppler:  <math>RIMP = (IVRT + IVCT)/ET = (TCO - ET)/ET</math></p>	<ul style="list-style-type: none"> <li>• Less affected by heart rate</li> <li>• Single-beat recording with no need for R-R interval matching</li> </ul>	<ul style="list-style-type: none"> <li>• Unreliable when RA pressure is elevated</li> </ul>
<p><b>RV global systolic function</b> FAC</p> 	<p>RV FAC in RV-focused apical four-chamber view:  <math>RV FAC (\%) = 100 \times (EDA - ESA)/EDA</math></p>	<ul style="list-style-type: none"> <li>• Established prognostic value</li> <li>• Reflects both longitudinal and radial components of RV contraction</li> <li>• Correlates with RV EF by CMR</li> </ul>	<ul style="list-style-type: none"> <li>• Neglects the contribution of RV outflow tract to overall systolic function</li> <li>• Only fair inter-observer reproducibility</li> </ul>
<p>EF</p> 	<p>Fractional RV volume change by 3D TTE:  <math>RV EF (\%) = 100 \times (EDV - ESV)/EDV</math></p>	<ul style="list-style-type: none"> <li>• Includes RV outflow tract contribution to overall function</li> <li>• Correlates with RV EF by CMR</li> </ul>	<ul style="list-style-type: none"> <li>• Dependent on adequate image quality</li> <li>• Load dependency</li> <li>• Requires offline analysis and experience</li> <li>• Prognostic value not established</li> </ul>

**Table 9 (Continued)**

Echocardiographic imaging	Recommended methods	Advantages	Limitations
<p><b>RV longitudinal systolic function</b> TAPSE</p> 	<ul style="list-style-type: none"> <li>• Tricuspid annular longitudinal excursion by M-mode (mm), measured between end-diastole and peak systole</li> <li>• Proper alignment of M-mode cursor with the direction of RV longitudinal excursion should be achieved from the apical approach.</li> </ul>	<ul style="list-style-type: none"> <li>• Established prognostic value</li> <li>• Validated against radionuclide EF</li> </ul>	<ul style="list-style-type: none"> <li>• Angle dependency</li> <li>• Partially representative of RV global function*</li> </ul>
<p><b>Pulsed tissue Doppler S wave</b></p> 	<ul style="list-style-type: none"> <li>• Peak systolic velocity of tricuspid annulus by pulsed-wave DTI (cm/sec), obtained from the apical approach, in the view that achieves parallel alignment of Doppler beam with RV free wall longitudinal excursion</li> </ul>	<ul style="list-style-type: none"> <li>• Easy to perform</li> <li>• Reproducible</li> <li>• Validated against radionuclide EF</li> <li>• Established prognostic value</li> </ul>	<ul style="list-style-type: none"> <li>• Angle dependent</li> <li>• Not fully representative of RV global function, particularly after thoracotomy, pulmonary thromboendarterectomy or heart transplantation</li> </ul>
<p><b>Color tissue Doppler S wave</b></p> 	<ul style="list-style-type: none"> <li>• Peak systolic velocity of tricuspid annulus by color DTI (cm/sec)</li> </ul>	<ul style="list-style-type: none"> <li>• Sampling is performed after image acquisition</li> <li>• Allows multisite sampling on the same beat</li> </ul>	<ul style="list-style-type: none"> <li>• Angle dependent</li> <li>• Not fully representative of RV global function, particularly after thoracotomy, pulmonary thromboendarterectomy or heart transplantation</li> <li>• Lower absolute values and reference ranges than pulsed DTI S' wave</li> </ul>

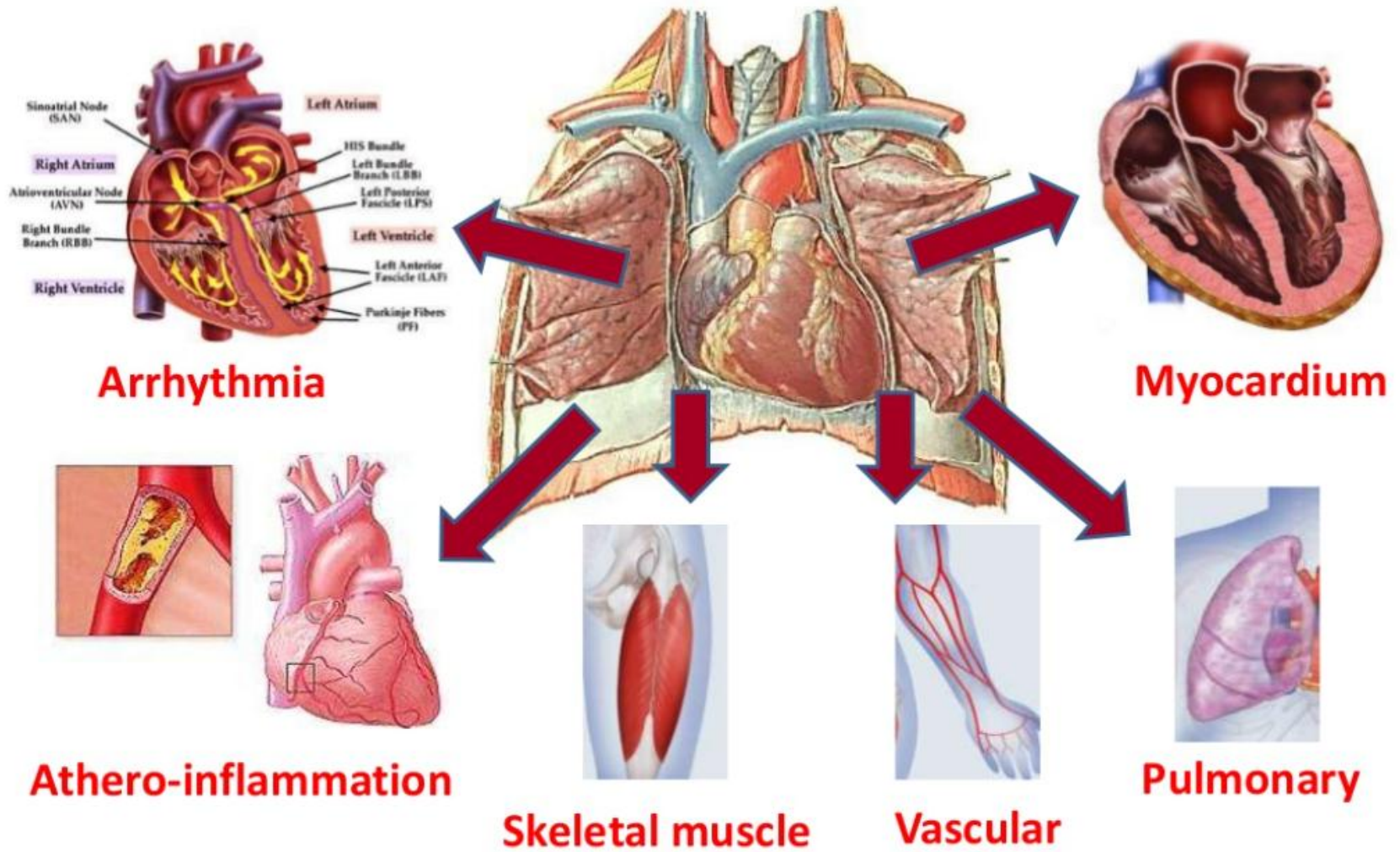
# Pitfalls

- However, all the above methods only provide indirect clues to estimate RV systolic function
- RV ejection fraction is difficult to be estimated from 2D Echo due to its complex geometry
- 3D Echo may provide new insight on volumetric assessment of RV

# Stage A HF – can we detect subclinical abnormalities?

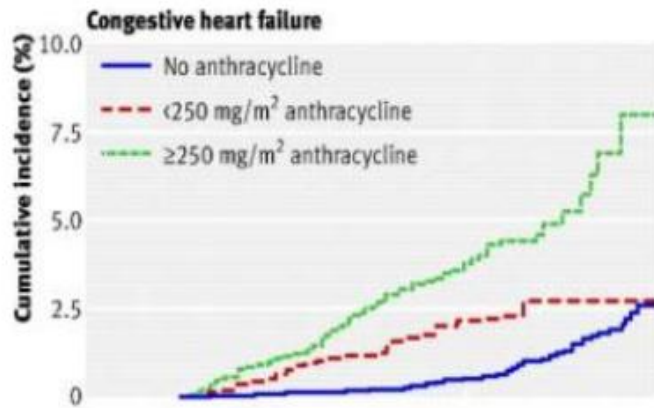
Classification	Severity				
	← Low <span style="float: right;">High</span> →				
ACC/AHA heart failure stage	<b>Stage A</b>	<b>Stage B</b>	<b>Stage C</b>		<b>Stage D</b>
	At risk (e.g., patients receiving cardiotoxins) but without structural heart disease or symptoms	Structural heart disease (hypertrophy, low EF, valve disease) but without signs or symptoms	Structural heart disease with prior or current symptoms		Refractory HF requiring specialized interventions
NYHA symptom classification	<b>Grade I</b>		<b>Grade II</b>	<b>Grade III</b>	<b>Grade IV</b>
	No limitation of activity		Mild limitation of activity	Marked limitation of activity	Confined to bed or chair

# Example: Oncology treatment side effects on CV system

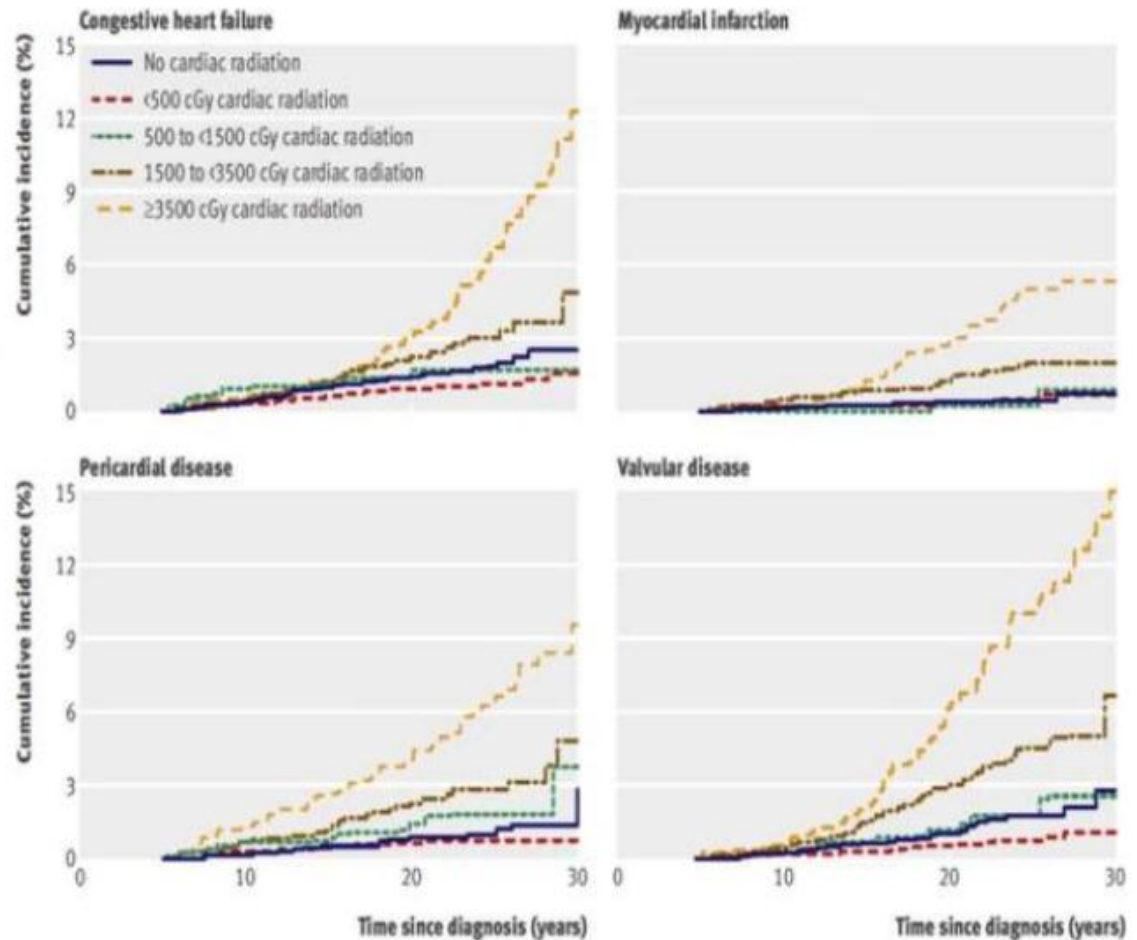


# Long term incidence of CV disease in treated patients

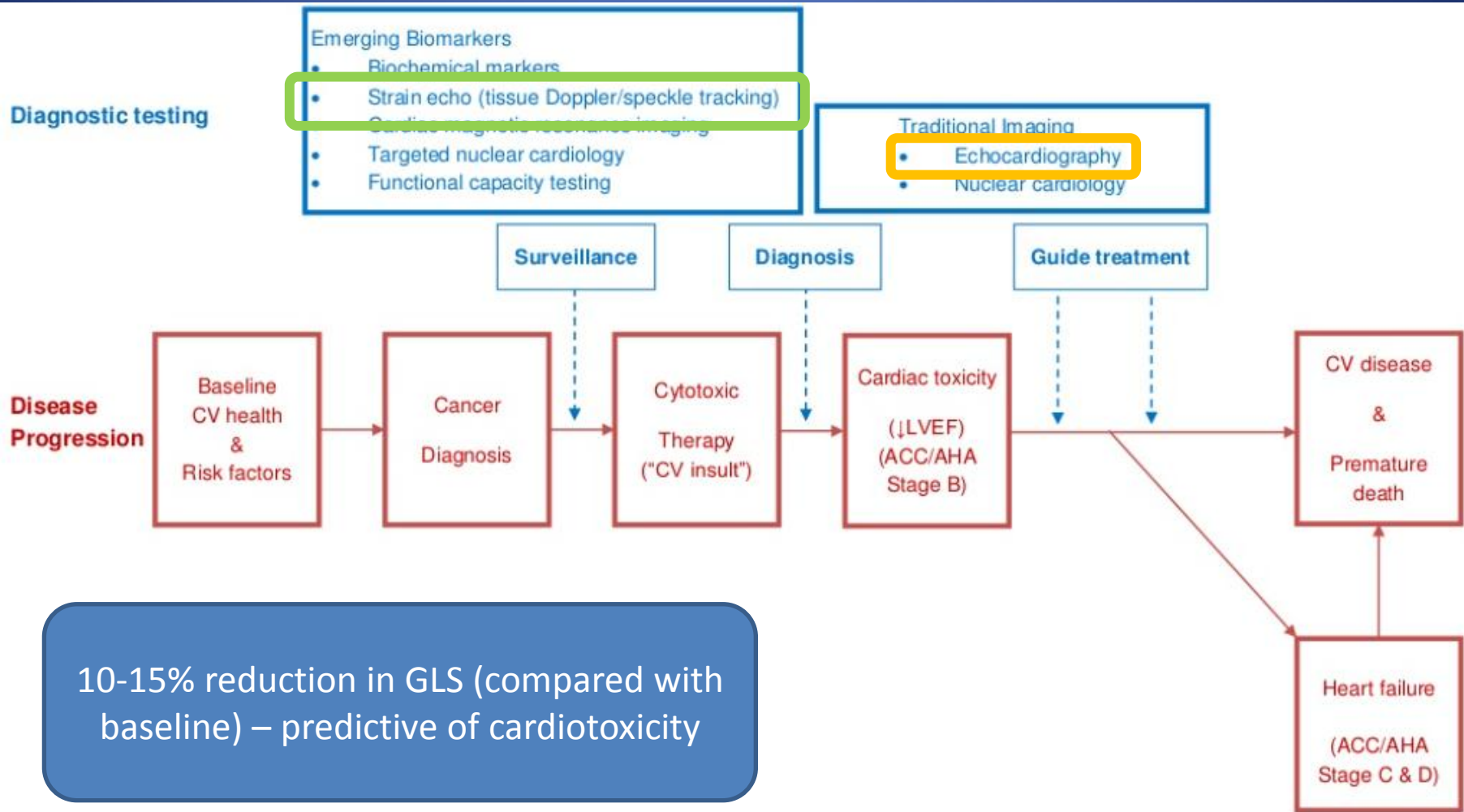
## Anthracyclines



## Radiation Therapy



# Early detection

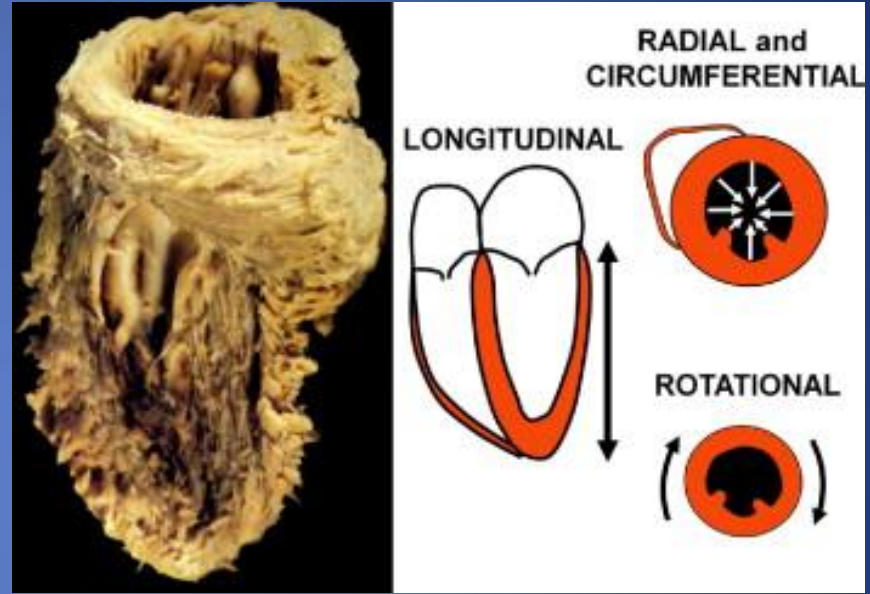
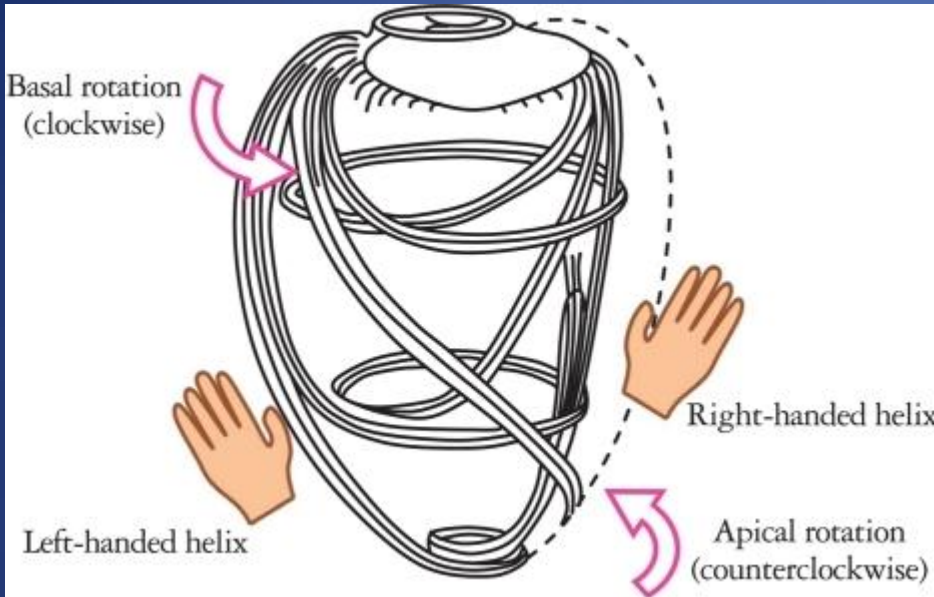




# Limitation of traditional 2D Echo

- LVEF
  - only tells you the “change of cavity” as end result
  - no information regarding the myocardial fiber contractile function
- Wall motion assessment
  - effect of “tethering” by adjacent normal segment
  - Appeared akinetic on 2D with 25% - 100% thickness myocardial injury / infarct

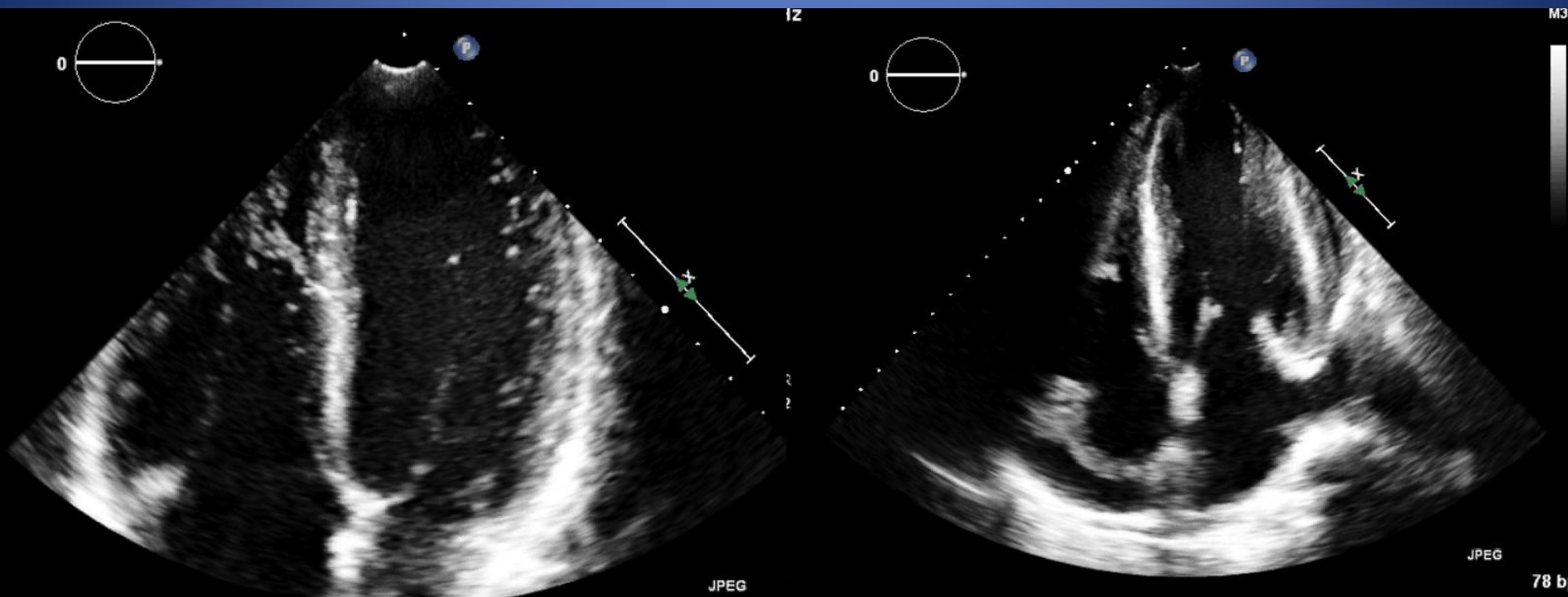
# Myocardial Deformation



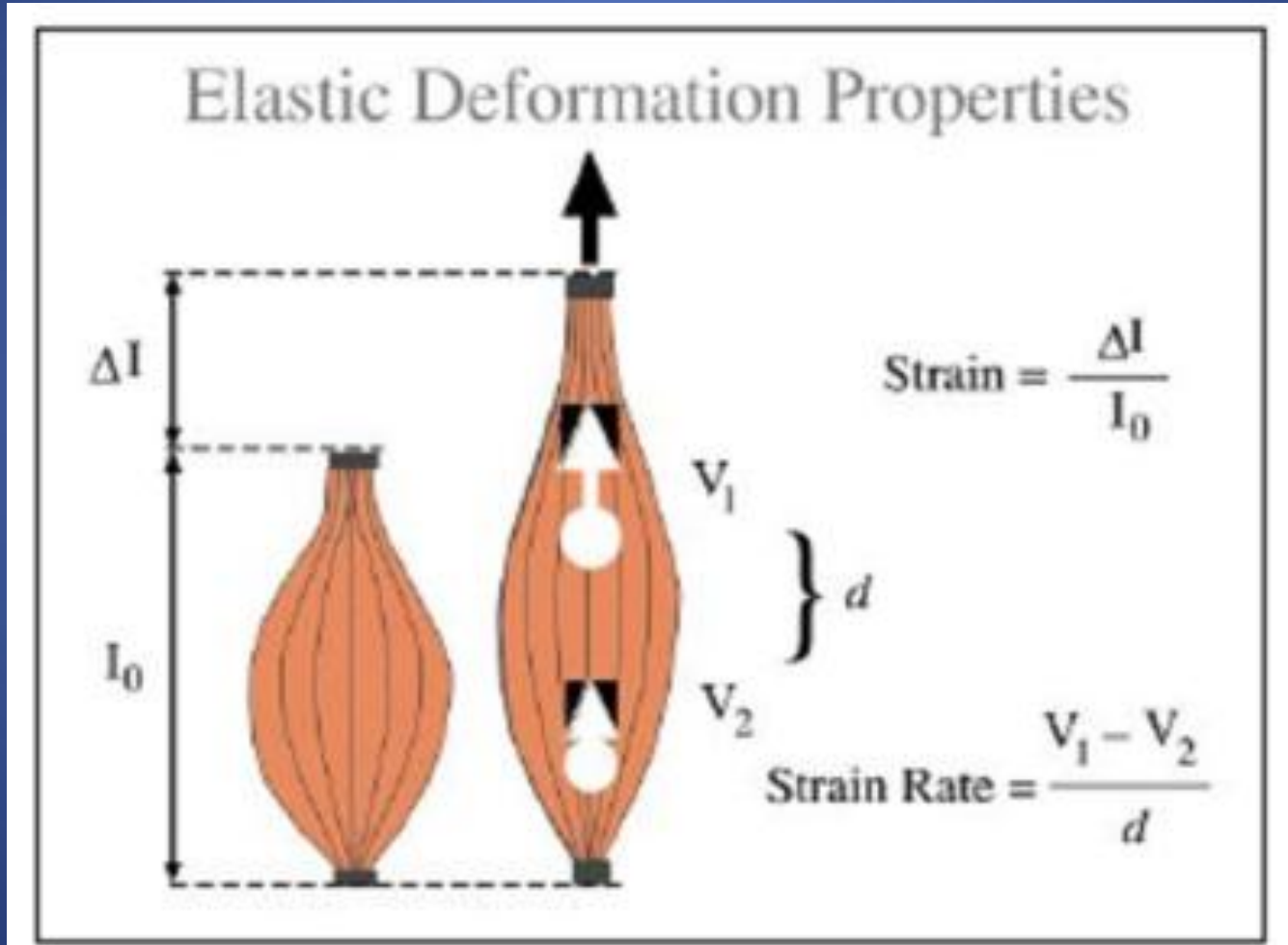
Subepicardium : helically left-handed direction  
Mid layer: run circumferentially  
Subendocardium: helically right-handed direction



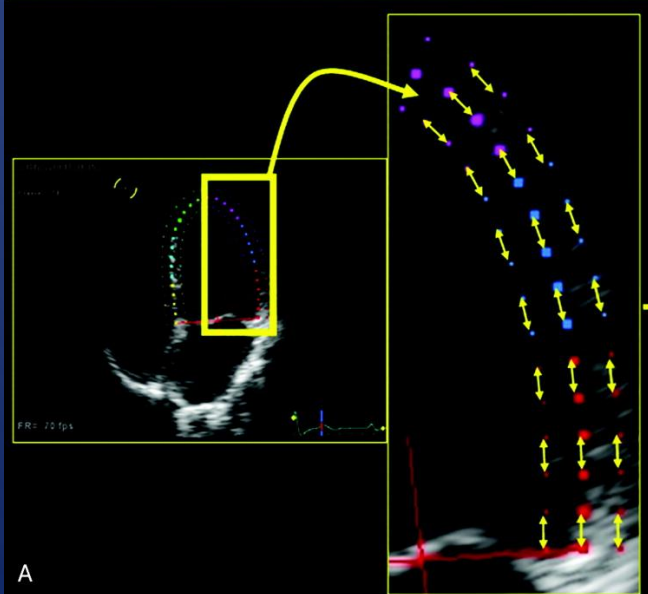
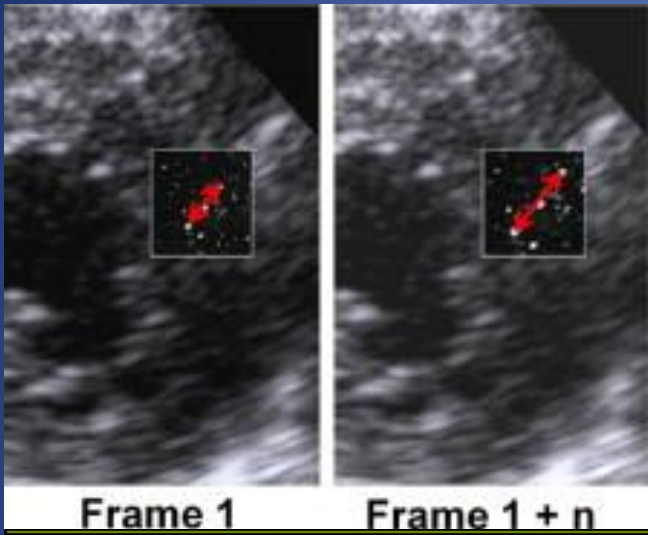
# Same LVEF, looks different?



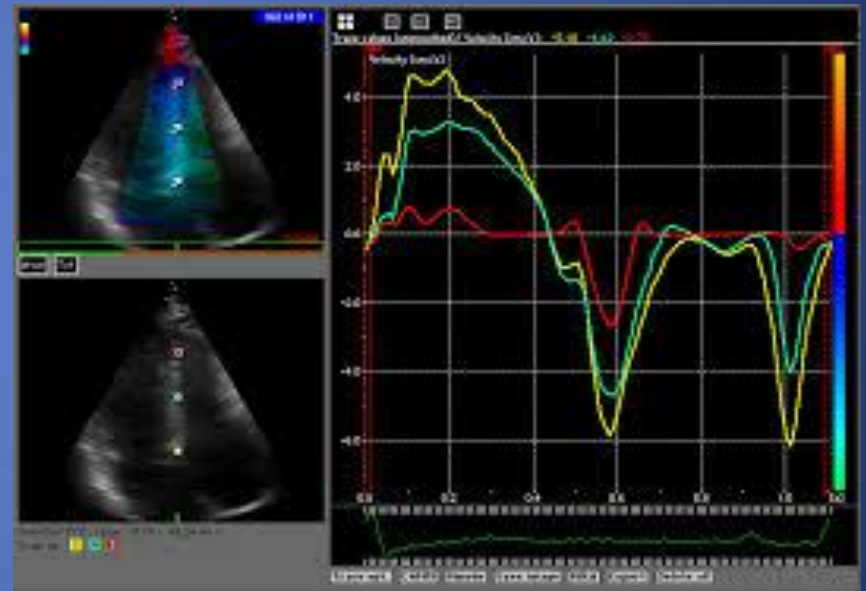
# Strain and Strain Rate

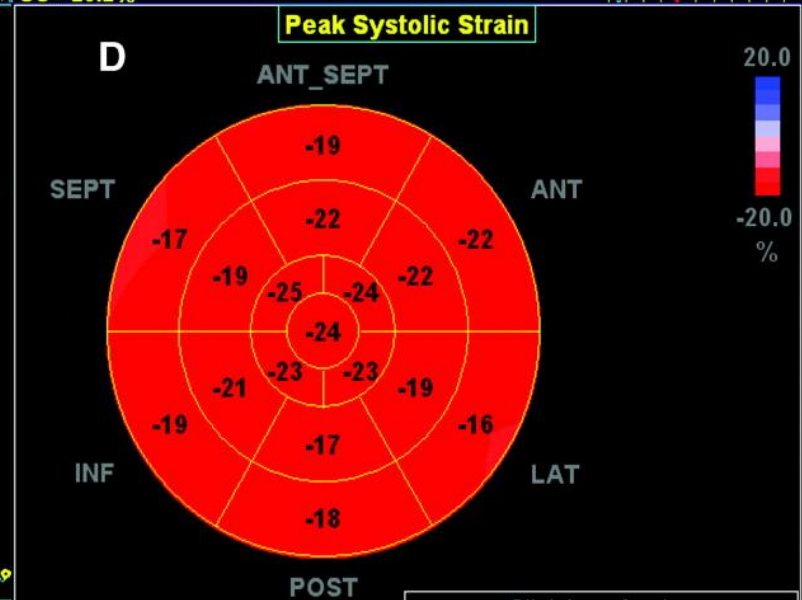
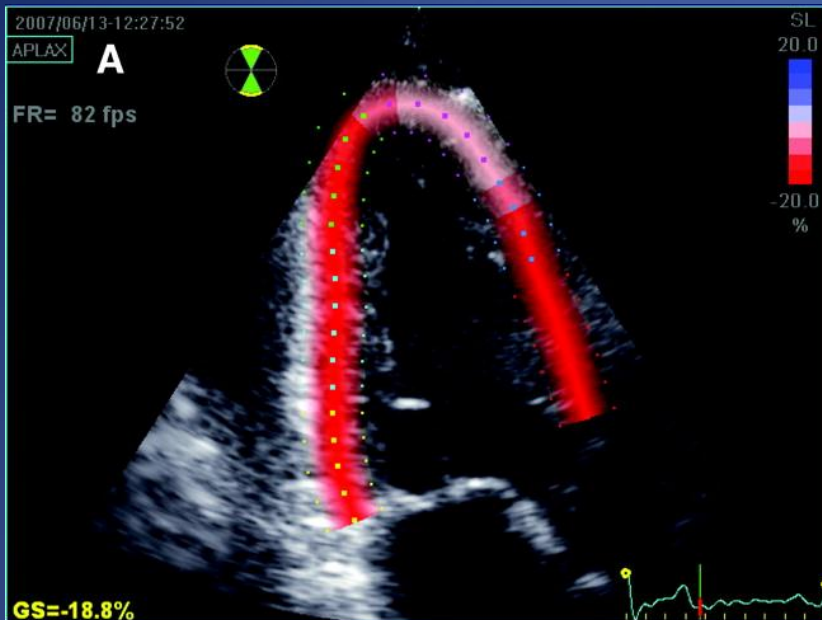


# Speckle Tracking

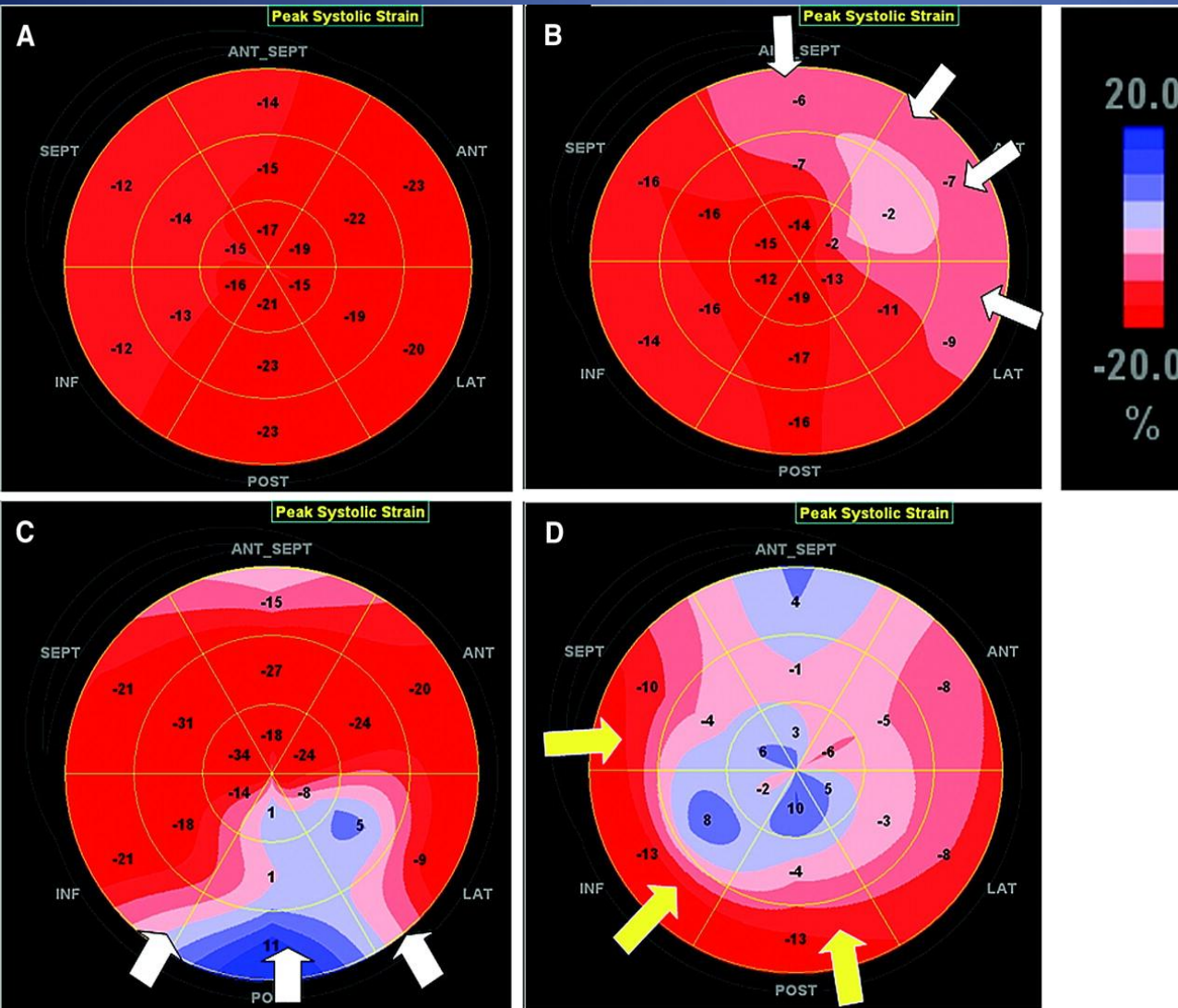


# Tissue doppler derived



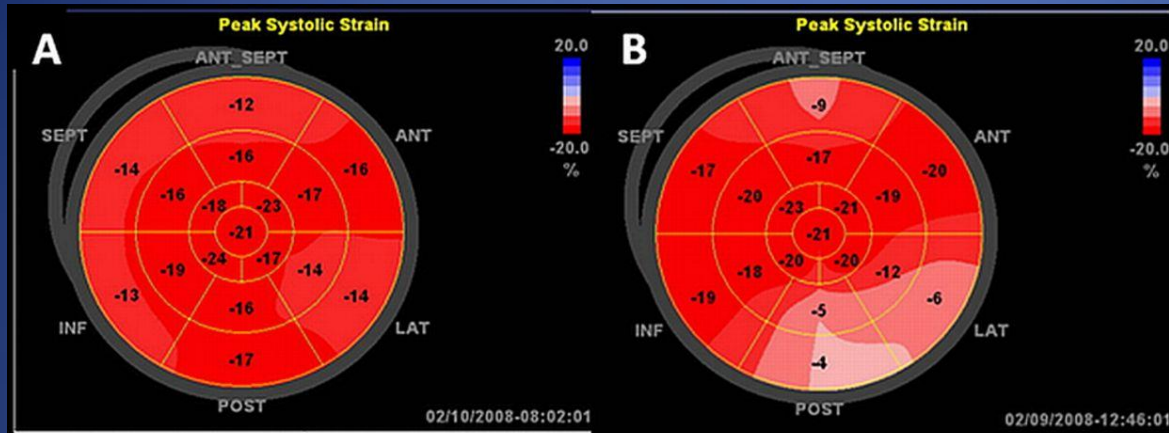


# Myocardial infarction

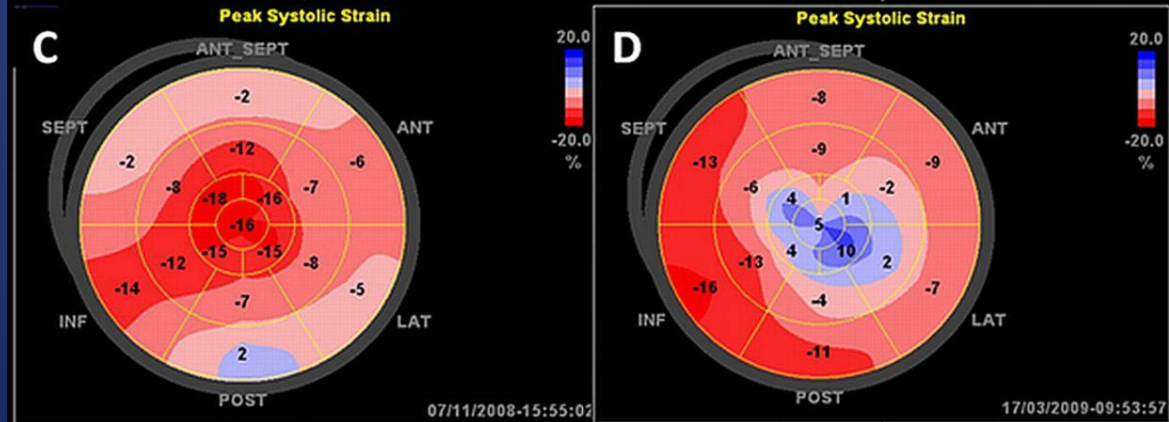


- A. Normal
- B. LAD infarct
- C. LCx infarct
- D. Non-ischaemic CMP

# Cardiomyopathies



GLPS_LAX	-16.1 %	AVC_AUTO	368 msec	GLPS_LAX	-9.7 %	AVC_AUTO	340 msec
GLPS_A4C	-14.8 %	HR_ApLAX	60.0 bpm	GLPS_A4C	-17.3 %	HR_ApLAX	57.4 bpm
GLPS_A2C	-19.3 %			GLPS_A2C	-20.0 %		
GLPS_Avg	-16.7 %			GLPS_Avg	-15.7 %		

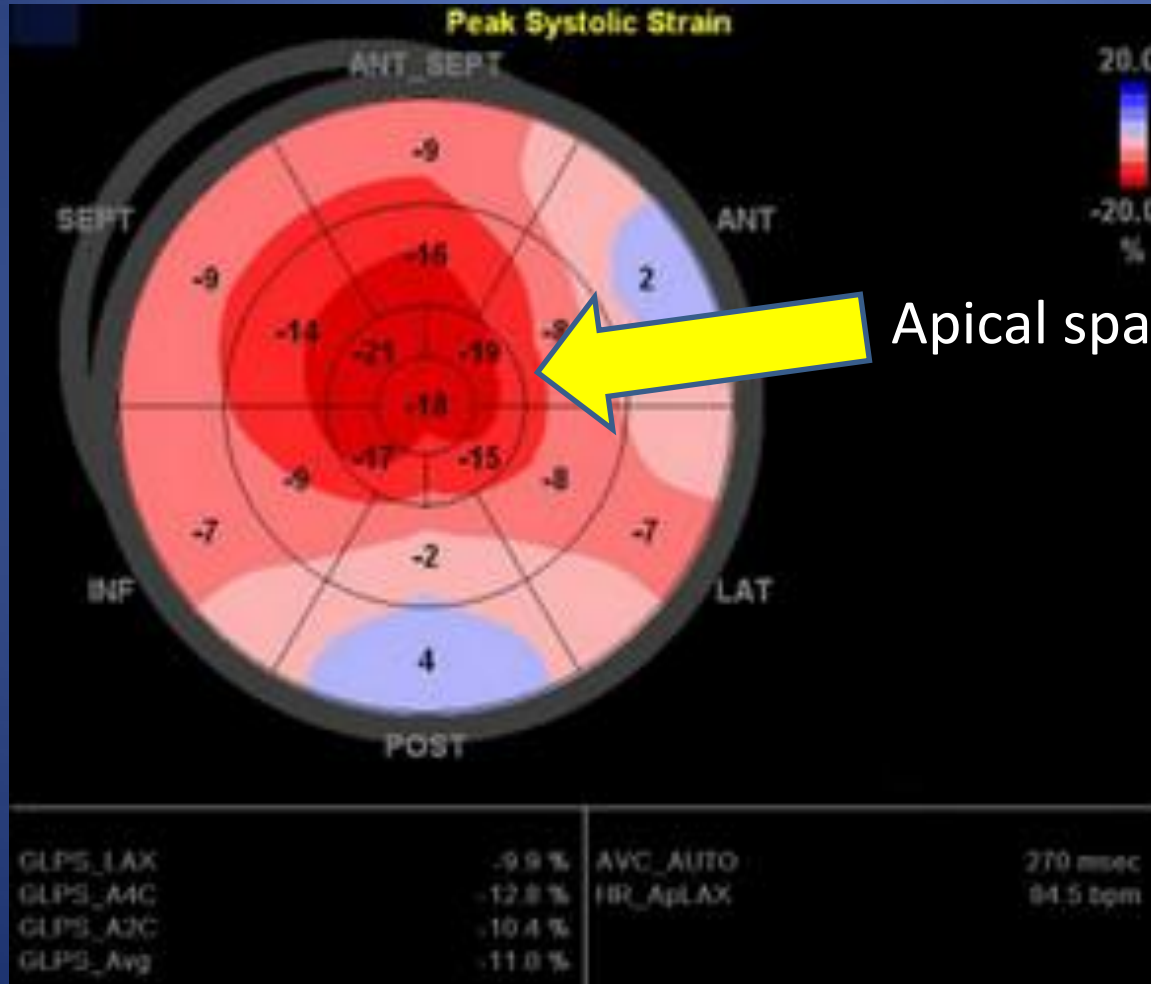


GLPS_LAX	-12.7 %	AVC_MEAS	366 msec	GLPS_LAX	-5.6 %	AVC_MEAS	379 msec
GLPS_A4C	-12.0 %	HR_ApLAX	55.2 bpm	GLPS_A4C	0.0 %	HR_ApLAX	55.4 bpm
GLPS_A2C	-12.6 %			GLPS_A2C	-8.0 %		
GLPS_Avg	-12.4 %			GLPS_Avg	-4.5 %		

- A. Normal athlete
- B. Hypertensive heart
- C. Hypertrophic cardiomyopathy
- D. Apical variant HCM



# Amyloid heart disease



# Ischaemic CMP

- Perfusion abnormalities
- Viability
- Guide decision on revascularization

# Exercise vs pharmacological stress Echo

	<b>Advantages</b>	<b>Disadvantages</b>
<b>Treadmill</b>	Widely available High workload	Post stress images Mild ischemia may revert
<b>Upright bicycle</b>	Imaging during exercise	Technically difficult
<b>Supine bicycle</b>	Imaging during exercise Dopplers readily available	Low workload
<b>Dobutamine</b>	Continuous imaging	Side effects
<b>Dipyridamole</b>	Continuous imaging	Side effects

# Stress Echo Interpretation

Interpretation	Rest / Baseline	Low dose stress	Peak & post stress
Normal	Normal	Normal	Hyperdynamic
Ischemic	Normal	Normal / severe ischemia – new RWMA	Decreased
Scar	WMA	No change	No change
Hibernating	WMA	Improved	Worsens
Stunned	WMA	Improved	Improved

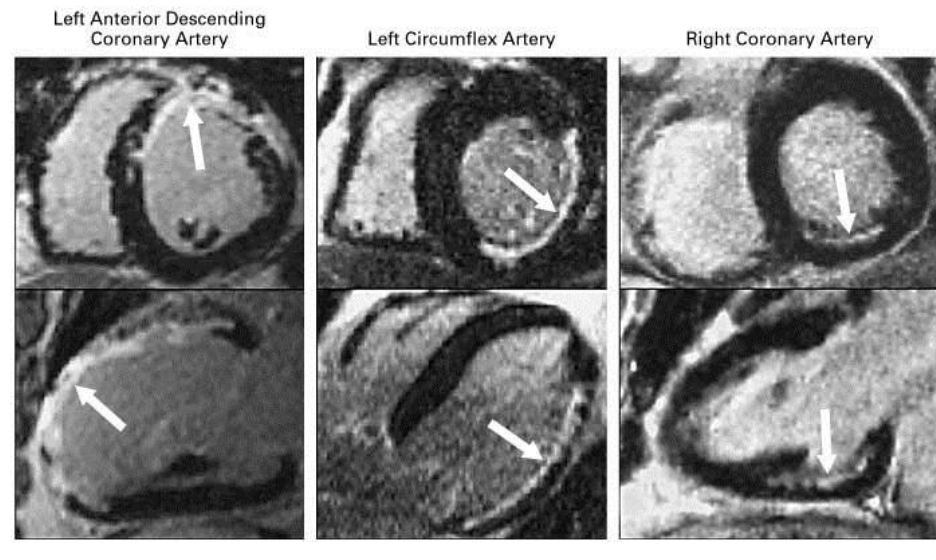
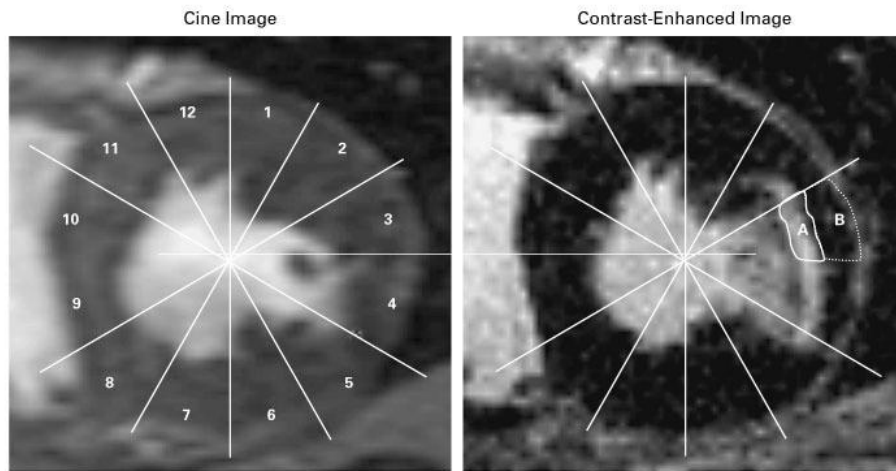
# Stress Echo – other parameters

- Change in diastolic function
- Change in RSVP
- Change in LV chamber size
- Change in haemodynamics in valvular disease
  - “mild MS” at rest with exertional symptoms
  - “LFLG severe AS”

# Cardiac MRI

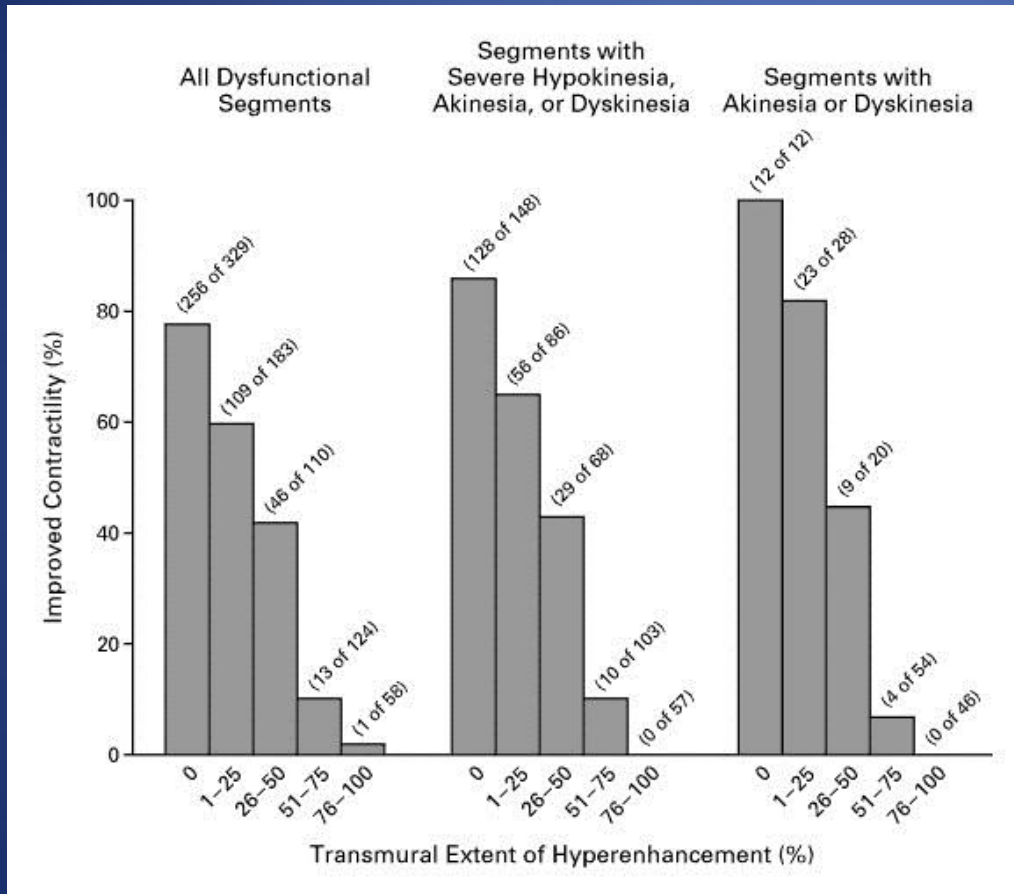
- Structure and function assessment
- Stress perfusion for ischaemia
- Late Gadolinium Enhancement (LGE)
  - Differentiating ischaemic vs non-ischaemic cause
  - Ischaemic – almost always involvement subendocardium or even transmural, corresponding to coronary artery territory

# LGE – transmural extent of infarct



*Kim, Raymond J., et al. "The use of contrast-enhanced magnetic resonance imaging to identify reversible myocardial dysfunction." New England Journal of Medicine 343.20 (2000): 1445-1453.*

# LGE – transmural extent of infarct



Can be used to predict whether or not regions of myocardial dysfunction will improve after revascularization.

Kim, Raymond J., et al. "The use of contrast-enhanced magnetic resonance imaging to identify reversible myocardial dysfunction." *New England Journal of Medicine* 343.20 (2000): 1445-1453.



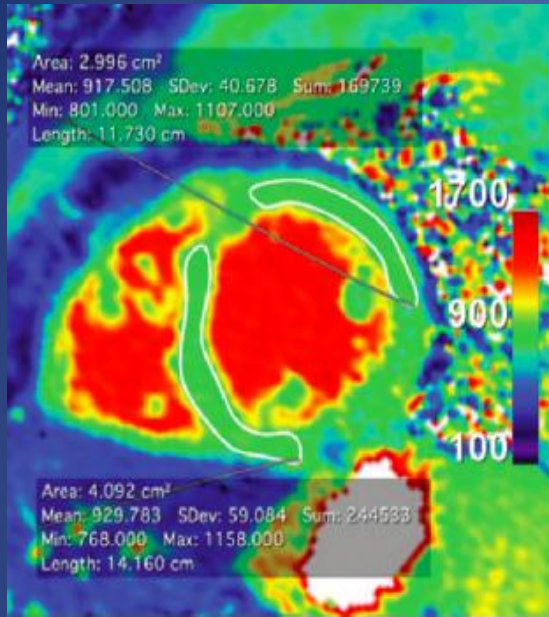
# LGE

- Predict response to CRT – transmural necrosis at inferolateral wall may do worse
- Predict arrhythmia risk base on extent of scarring

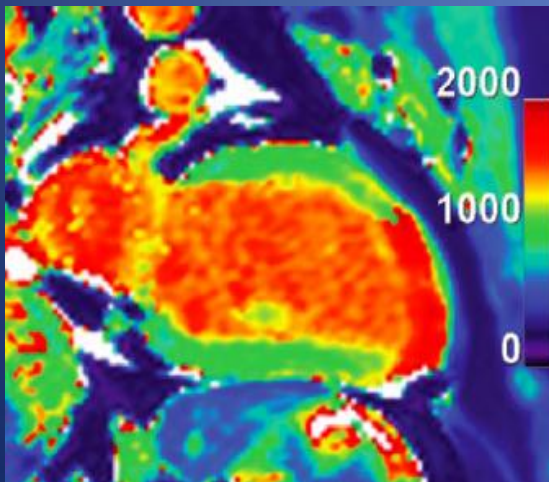
# Tissue characterization

- Native T1 – non-contrast
- Extracellular volume (ECV)
- T2: acute inflammation, edema, infarct
- T2\*

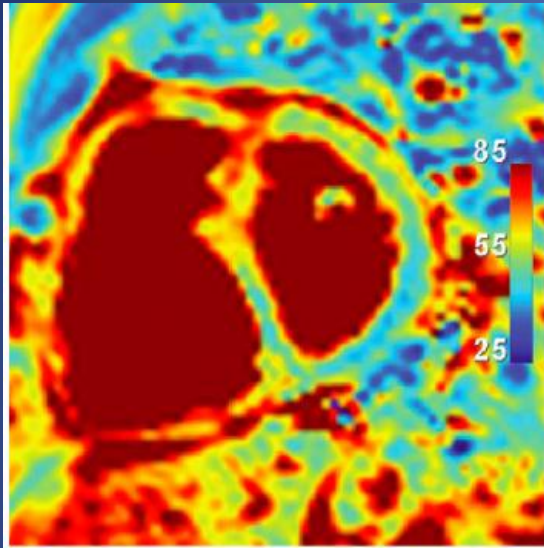
# Native T1 mapping



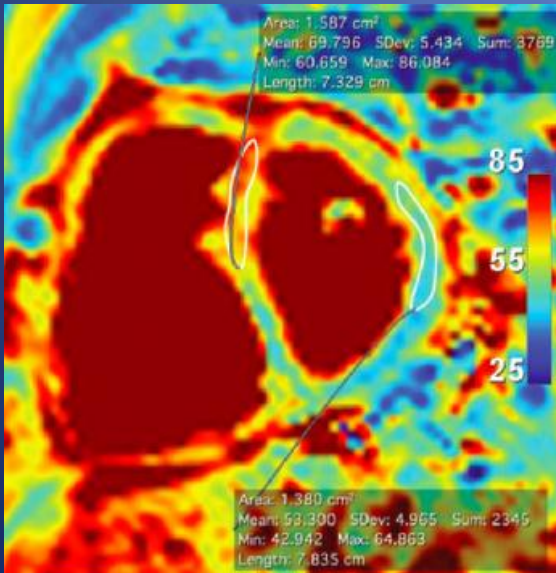
- Parametric mapping
- A more recent development in myocardial tissue characterisation
- Diffuse myocardial fibrosis -  $\uparrow$  T1 values
- Non-specific
  - any pathology resulting in edema/fibrosis/other depositional disease
- Values applicable to local setup only



# T2 mapping



- Similar principle to T1 mapping
- T2 relaxation time altered by water content
- Detect myocardial edema in different diseases
- “Area-at-risk” myocardium



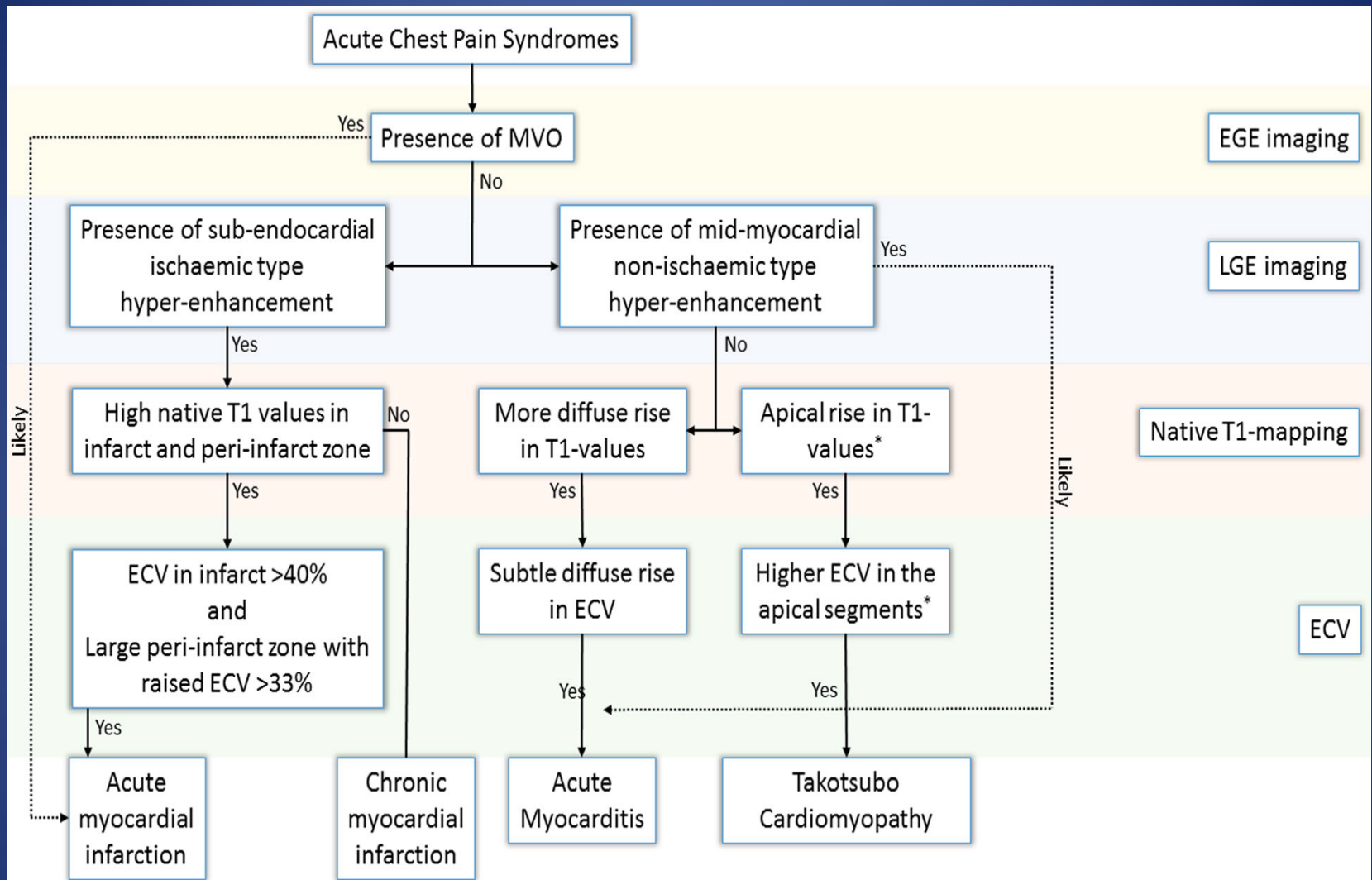
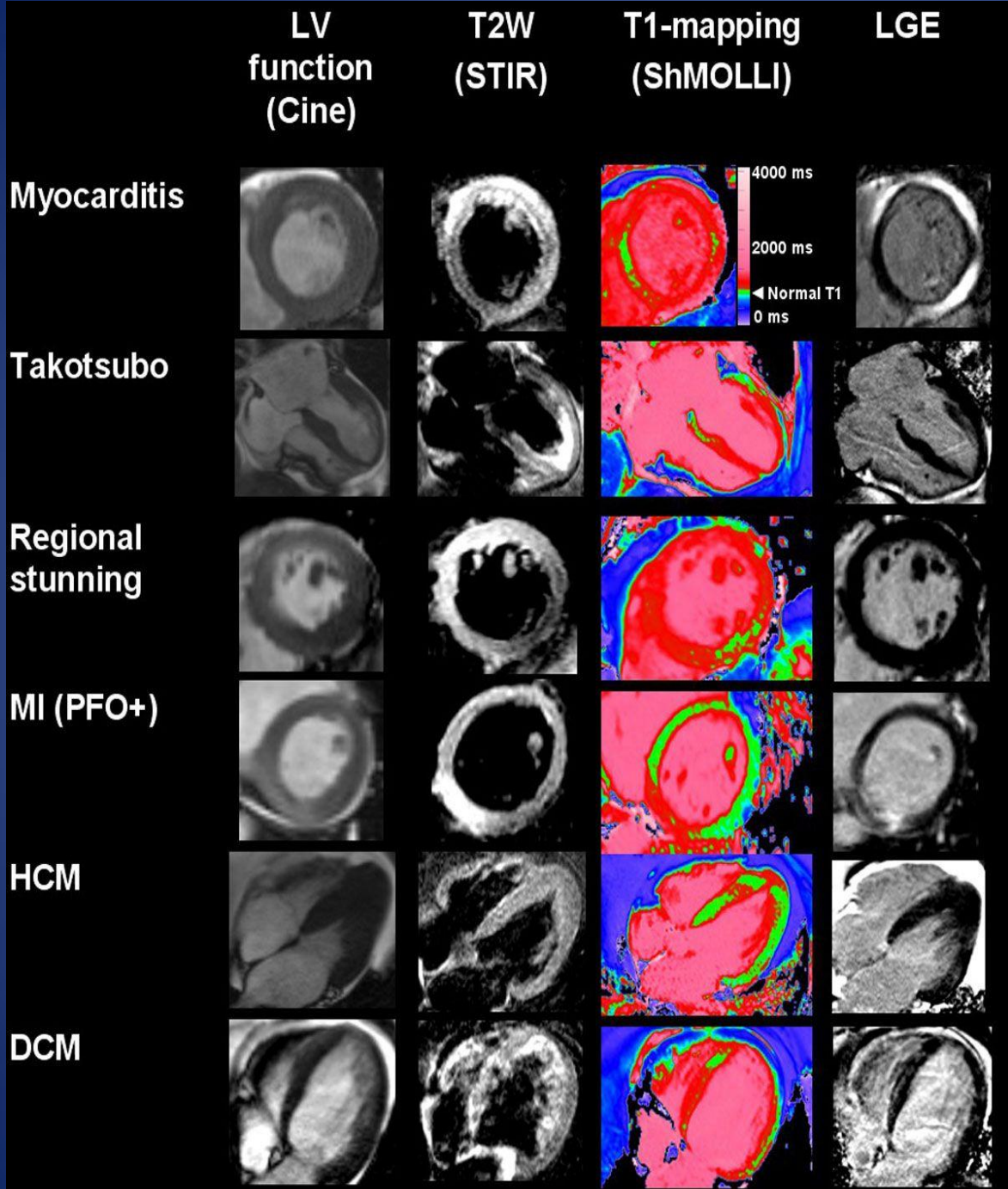


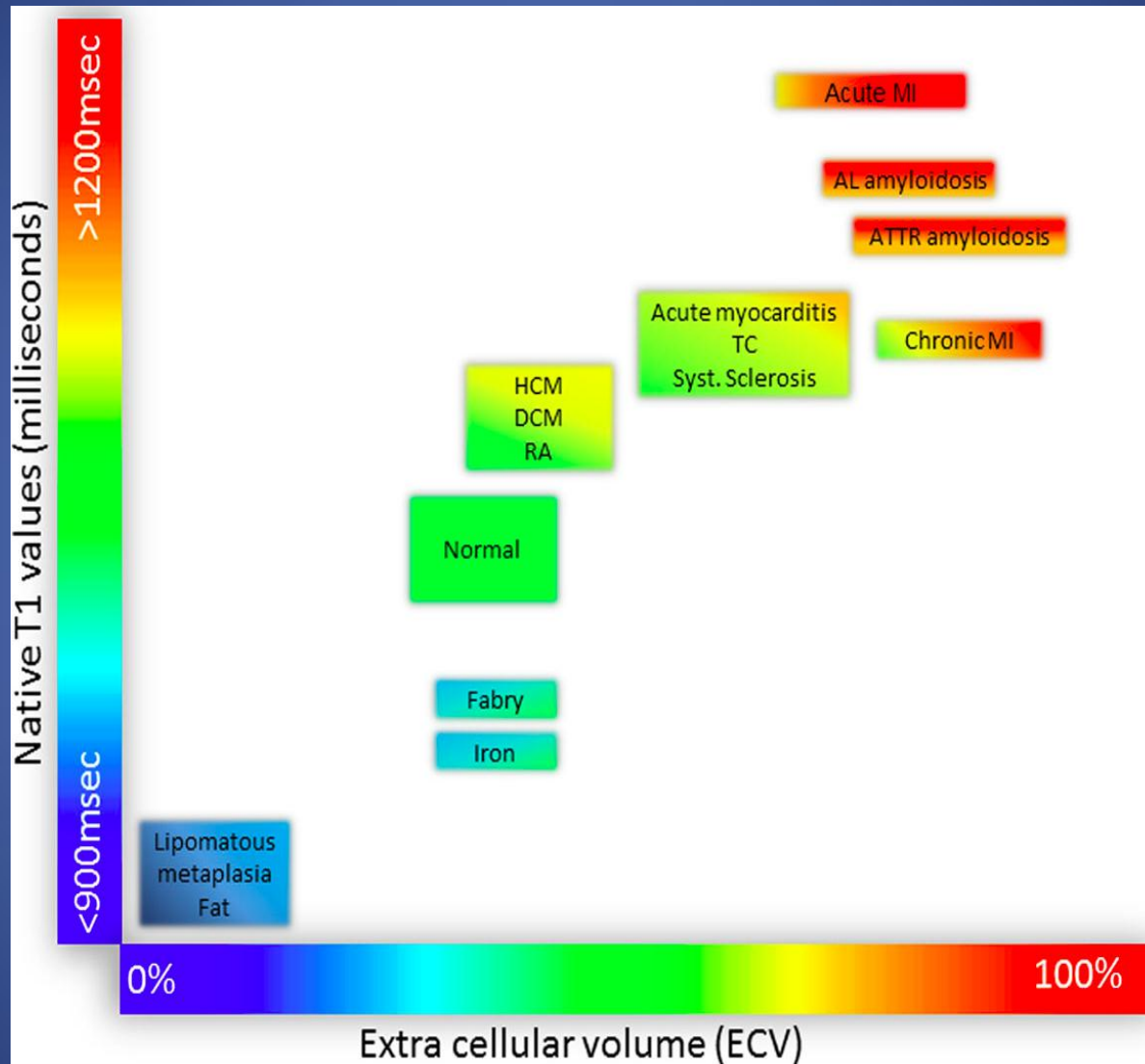
Fig. 3 Acute chest pain syndromes algorithm using multi-parametric tissue characterisation. ECV denotes extra-cellular volume, LGE Late Gadolinium Enhancement, and MVO microvascular obstruction. .

\*This holds true for classical type 1 Takotsubo Cardiomyopathy



Ferreira et al. Journal of Cardiovascular Magnetic Resonance 2014 16 (Suppl 1) :P215

# T1 mapping and ECV in clinical practice

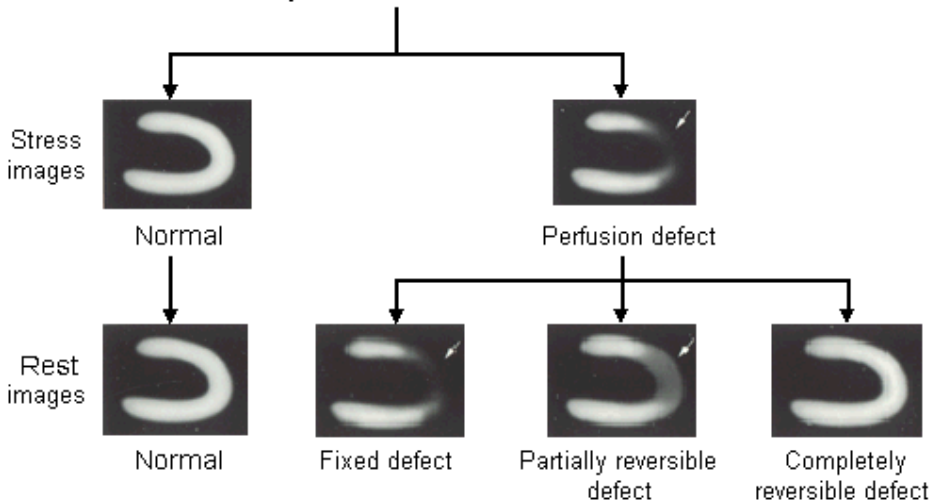


# Nuclear imaging for ischaemia

- Thallium-201 or technetium-99m
- Exercise or pharmacological stress
- Evaluate ischaemia, infarction and viability
- Prior studies suggest excellent negative predictive values but poor positive predictive values
- Ischaemic CMP shows more extensive, diffuse and severe perfusion defects than NICM, but a noteworthy degree of overlap exists



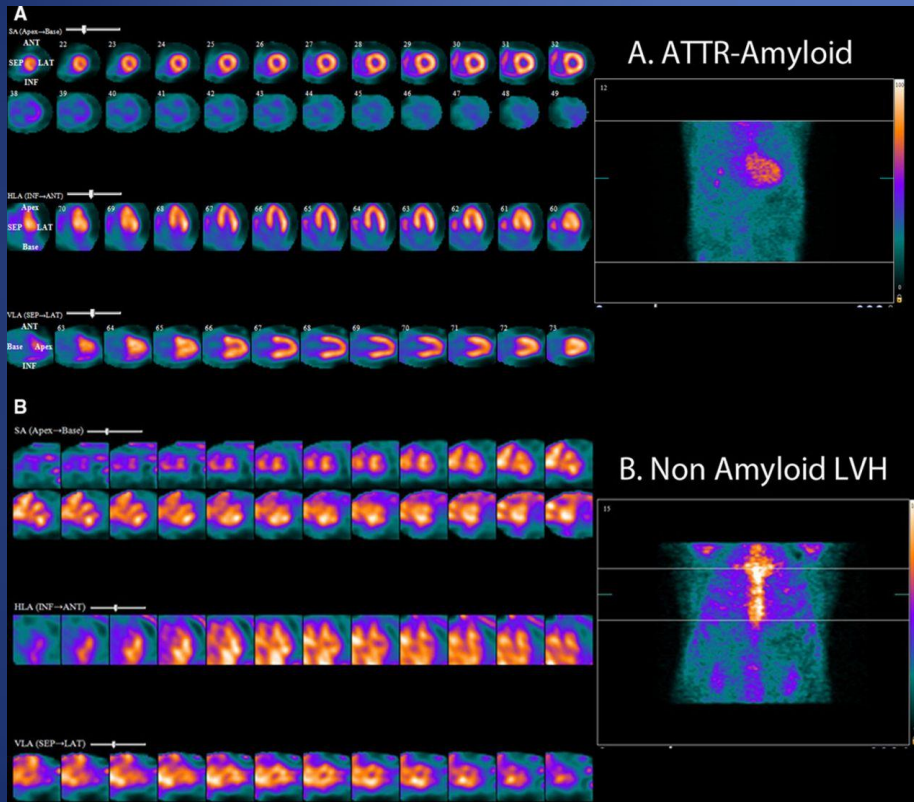
Injection of radiotracer



		Stress	Rest or redist	Late redist*
Normal	$^{99m}\text{Tc}$ or $^{201}\text{Tl}$			
Reversible	$^{99m}\text{Tc}$ or $^{201}\text{Tl}$			
Mixed	$^{99m}\text{Tc}$ or $^{201}\text{Tl}$			
Partially reversible	$^{99m}\text{Tc}$ or $^{201}\text{Tl}$			
Fixed	$^{99m}\text{Tc}$ or $^{201}\text{Tl}$			
Late reversible	$^{201}\text{Tl}$ only			
Reverse redistribution**	$^{201}\text{Tl}$ only			

Source: Valentin Fuster, Robert A. Harrington, Jagat Narula, Zubin J. Eapen: Hurst's The Heart, Fourteenth Edition: www.accessmedicine.com Copyright © McGraw-Hill Education. All rights reserved.

# Nuclear imaging for cardiac amyloidosis



- direct amyloid imaging agents (I-123–labeled serum amyloid P component),
- bone imaging agents (Tc-99m pyrophosphate or Tc-99m 3,3-diphosphono-1,2-propanodicarboxylic acid [DPD])
- agents to image cardiac sympathetic innervation (I-123 metaiodobenzylguanidine)

How to Image Cardiac Amyloidosis, Volume: 7, Issue: 3,  
Pages: 552-562, DOI: (10.1161/CIRCIMAGING.113.001396)

Table 1: Main Indications and Applications for Each One of the Available Imaging Modalities in the Assessment of Heart Failure Patients

	2D ECO	3DE	Strain	Cardiovascular Magnetic Resonance	Nuclear	Computed Tomography
LV/RV volumes	RU	AI		AI (GS)		AI
LV systolic function	RU	AI	AI	AI (GS)		
LV diastolic function	RU (GS)		AI	AI		
RV function	RU	AI	AI	AI (GS)		
Ischaemia	RU		AI	AI (GS)	AI (GS)	
Viability	RU		AI	AI (GS)	AI (GS)	
Cardiomyopathies and other heart failure aetiologies	RU		AI	AI (GS)		AI
Risk assessment (arrhythmia)						
Therapy guidance (cardiac resynchronisation therapy)						
Follow-up	RU					

Green: best performance of the technique for this indication; yellow: the technique could provide useful information for this indication; red: no/little use for this indication. AI = provides additional information to that obtained with 2D echocardiogram; GS = gold standard; RU = routinely used for this indication. LV = left ventricular; RV = right ventricular.

# Imaging in Heart Failure

- Echo continues to be the method of choice for its availability, cost and usefulness, it provides most of the information required for the management and follow up of HF patients and it has been enhanced with the development of 3DE and strain.
- Cardiac MRI and nuclear imaging are alternative for ischaemia or viability assessment
- Cardiac MRI is excellent in tissue characterization to differentiate different types of cardiomyopathies